



Get Clarity On Generics

Cost-Effective CT & MRI Contrast Agents

 FRESENIUS
KABI

[WATCH VIDEO](#)

AJNR

This information is current as
of August 23, 2025.

Velocity Measurements in the Middle Cerebral Arteries of Healthy Volunteers Using 3D Radial Phase-Contrast HYPRFlow: Comparison with Transcranial Doppler Sonography and 2D Phase-Contrast MR Imaging

W. Chang, B. Landgraf, K.M. Johnson, S. Kecskemeti, Y. Wu, J. Velikina, H. Rowley, O. Wieben, C. Mistretta and P. Turski

AJNR Am J Neuroradiol 2011, 32 (1) 54-59

doi: <https://doi.org/10.3174/ajnr.A2240>

<http://www.ajnr.org/content/32/1/54>

ORIGINAL
RESEARCH

W. Chang
B. Landgraf
K.M. Johnson
S. Kecskemeti
Y. Wu
J. Velikina
H. Rowley
O. Wieben
C. Mistretta
P. Turski



Velocity Measurements in the Middle Cerebral Arteries of Healthy Volunteers Using 3D Radial Phase-Contrast HYPRFlow: Comparison with Transcranial Doppler Sonography and 2D Phase-Contrast MR Imaging

BACKGROUND AND PURPOSE: We have developed PC HYPRFlow, a comprehensive MRA technique that includes a whole-brain CE dynamic series followed by PC velocity-encoding, yielding a time series of high-resolution morphologic angiograms with associated velocity information. In this study, we present velocity data acquired by using the PC component of PC HYPRFlow (PC-VIPR).

MATERIALS AND METHODS: Ten healthy volunteers (6 women, 4 men) were scanned by using PC HYPRFlow and 2D-PC imaging, immediately followed by velocity measurements by using TCD. Velocity measurements were made in the M1 segments of the MCAs from the PC-VIPR, 2D-PC, and TCD examinations.

RESULTS: PC-VIPR showed approximately 30% lower mean velocity compared with TCD, consistent with other comparisons of TCD with PC-MRA. The correlation with TCD was $r = 0.793$, and the correlation of PC-VIPR with 2D-PC was $r = 0.723$.

CONCLUSIONS: PC-VIPR is a technique capable of acquiring high-resolution MRA of diagnostic quality with velocity data comparable with TCD and 2D-PC. The combination of velocity information and fast high-resolution whole-brain morphologic angiograms makes PC HYPRFlow an attractive alternative to current MRA methods.

ABBREVIATIONS: CE = contrast-enhanced; CE-VIPR = contrast-enhanced vastly undersampled isotropic projection reconstruction; 2D-PC = 2D phase-contrast; HYPR-LR = highly constrained local projection reconstruction; MCA = middle cerebral artery; MRA = MR angiography; PC = phase-contrast; PC HYPRFlow = time-resolved MRA using highly constrained projection reconstruction and PC-VIPR data for the reconstruction convolution; PC-MRA = phase-contrast MR angiography; PC-VIPR = phase-contrast vastly undersampled isotropic projection reconstruction; SNR = signal intensity-to-noise ratio; TCD = transcranial Doppler sonography; VENC = velocity encoding; WSS = wall shear stress

The acquisition of intracranial velocity measurements and velocity derivatives (WSS) is clinically useful for the evaluation of neurovascular disorders such as vasospasm, stenoses, and aneurysms, but measurement of intracranial velocity has proved challenging. TCD has been used clinically for decades and allows the acquisition of velocity measurements in the MCAs and several other vessels through the temporal window. However, the sonic properties of the cranial vault prevent measurement of velocity in many intracranial arteries by TCD. 2D-PC MR imaging has been used to obtain hemodynamic data for the past 20 years but has limited coverage and

exhibits partial volume effects.¹ 3D and 4D methods have higher SNR, fewer partial volume effects, and improved spatial resolution but have an increased scanning time.² Previous implementation of whole-brain cardiac-gated PC Cartesian 4D MR imaging has resulted in scanning times too long to be clinically useful.^{3,4} Advances in PC Cartesian acquisition have reduced scanning times and increased resolution to some degree. Investigators have used view-sharing,⁵ spatial harmonics,⁶ and parallel imaging⁷ to reduce scanning time. With these methods, in-plane spatial resolutions on the order of 0.6×1 mm with scanning times in the 8- to 12-minute range can be achieved.⁸

However, obtaining high-resolution whole-brain angiograms with velocity information within clinically useful imaging times has been challenging. Recently, we implemented radial imaging techniques that are particularly well-suited for neurovascular MRA. Because MRA is sparse, consisting of few changing nonzero elements, accelerated acquisitions can often be performed with tolerable artifacts. For example, azimuthally undersampled radial acquisitions can be used to acquire images in much shorter scanning times than Cartesian acquisitions of a similar resolution with acceptable SNR and image quality,⁹ due to the rela-

Received March 15, 2010; accepted after revision June 1.

From the Departments of Medical Physics (K.M.J., S.K., Y.W., J.V., O.W., C.M.), Radiology (B.L., H.R., C.M., P.T.), and Biomedical Engineering (K.M.J., C.M.), University of Wisconsin, Madison, Wisconsin; and University of Wisconsin School of Medicine and Public Health (W.C.), Madison, Wisconsin.

This work was supported by National Institutes of Health grant R21 EB009441 to Patrick Turski.

Please address correspondence to Warren Chang, MD, University of Wisconsin School of Medicine and Public Health, 750 Highland Ave, Madison, WI 53705; e-mail: wmchang2@wisc.edu



Indicates open access to non-subscribers at www.ajnr.org

DOI 10.3174/ajnr.A2240

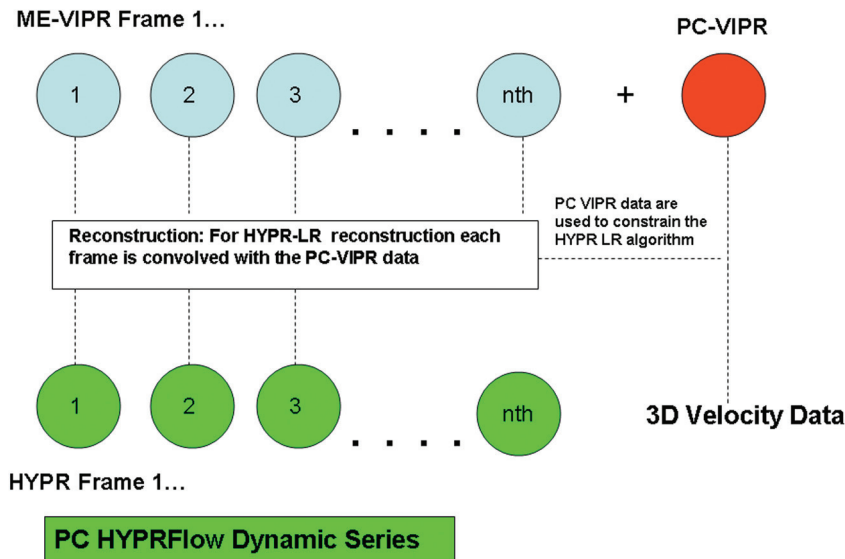


Fig 1. Flow chart of PC HYPRFlow. First a series of low-resolution CE source images is acquired, followed by a high-resolution velocity-encoded PC acquisition. Then the low-resolution source images are convolved with the high-resolution PC image by using HYPR-LR, resulting in a time series of high-resolution HYPR images.

tively benign nature of streaklike artifacts caused by the undersampling.^{10,11}

We have combined radial undersampling with a novel constrained image reconstruction technique to create PC HYPRFlow,^{9,12} a comprehensive MRA technique. Figure 1 shows a flow chart of how images are acquired and reconstructed by using PC HYPRFlow. A series of low-resolution 3D-radial CE source images are acquired (CE-VIPR), followed by a high-resolution velocity-encoded PC acquisition (PC-VIPR¹³). The low-resolution source images are then convolved with the high-resolution PC velocity acquisition by using a technique called HYPR-LR¹⁴ to yield a time series of high-resolution morphologic angiograms with associated velocity information. With current protocols, PC HYPRFlow provides whole-brain angiograms with excellent spatial resolution ($0.68 \times 0.68 \times 0.68 \text{ mm}^3$) with scanning times of 5–6 minutes.⁹

Because PC HYPRFlow is a highly accelerated technique, it may be susceptible to errors. To ensure diagnostic confidence, we have conducted several studies to validate image quality and velocity measurements from PC HYPRFlow.^{9,15–17} We previously reported that PC HYPRFlow provides images of diagnostic quality in medium- and large-sized intracranial vessels.⁹ In this study, we investigated velocity information acquired by using the PC component of PC HYPRFlow. We validated velocity measurements acquired by using PC-VIPR in the MCAs of healthy volunteers by comparing them with velocity measurements from 2 reference standards, TCD and Cartesian 2D-PC-MRA. The purpose of this comparison was to define the relationship of PC HYPRFlow velocity measurements to other established modalities.

Materials and Methods

Volunteer studies were performed in compliance with Health Insurance Portability and Accountability Act regulations and by using a protocol approved by the local institutional review board. Ten healthy volunteers ranging from 19 to 58 years of age were imaged (6 women, 4 men) with a clinical 3T MR imaging system (MR HD 750; GE

Healthcare, Milwaukee, Wisconsin) with a 8-channel head coil (Excite HD Brain Coil, GE Healthcare). Before contrast injection, a fast 2D-PC scan of each MCA was obtained to estimate the velocity to determine optimum VENC to prevent aliasing, followed by a PC HYPRFlow acquisition. Two fast low-resolution scans ($2 \times 2 \times 2 \text{ mm}^3$) were used in the time-resolved multiecho 3D radial acquisition (CE-VIPR).¹⁸ Contrast was injected during the second scan. Subsequently, velocity encoding was performed by using a high-resolution dual-echo 3D-radial PC acquisition (PC-VIPR). The PC-VIPR data were used as a composite image (angiographic constraint) for HYPR-LR reconstruction and for hemodynamic evaluation.¹⁴ Immediately following the MR imaging examination, the volunteers underwent TCD scanning.

MR Imaging Protocol

Imaging parameters for CE-VIPR were the following: FOV = $26 \times 26 \times 26 \text{ cm}^3$, TR/TE = 3.0/0.4 ms, bandwidth = 125 kHz. For each projection, there were 64 points from the center to the edge of the k -space, with a frame update time of 0.75 seconds. Scanning parameters for postcontrast PC-VIPR were the following: FOV = $22 \times 22 \times 22 \text{ cm}^3$, TR/TE = 12.5/4.8 ms, VENC = 80–150 cm/s, bandwidth = 83.3 kHz, readout matrix = 320 points per projection, spatial resolution for the composite image = $0.68 \times 0.68 \times 0.68 \text{ mm}^3$. Seven thousand projections were acquired within 5 minutes. Gadobenate dimeglumine (MultiHance; Bracco Diagnostics, Princeton, New Jersey) was injected at 3 mL/s, and the contrast dose was 0.1 mm/kg followed by a 20-mL saline flush. The MR imaging acquisitions were cardiac gated by using chest leads (Table).

A series of 3D time-resolved velocity images were reconstructed from the PC-VIPR data. A MatLab inhouse developed software filter with 50 ms at a low spatial frequency and 130 ms at a high spatial frequency was applied to improve the SNR. A vascular mask was generated by applying a signal-intensity threshold on the complex difference image. Subsequently, a region of interest, including approximately 100 voxels, was chosen in the M1 segment of the MCA as shown in Fig 2. Velocity measurements were made by using an in-house flow tool.¹⁹ Mean velocity was averaged within the region of interest for each time frame. Mean velocity through the whole cardiac

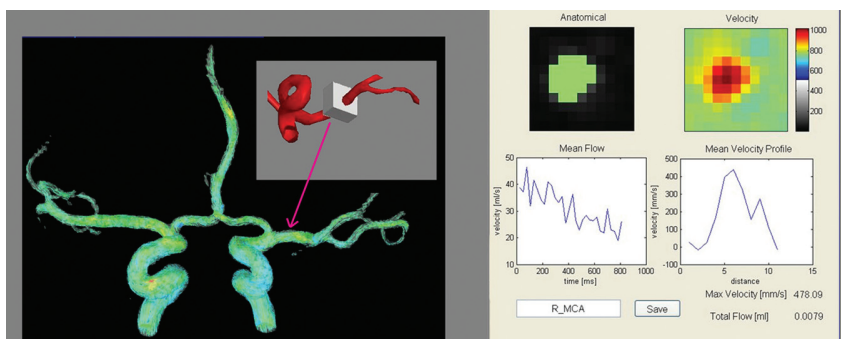


Fig 2. A 100-voxel box is selected in each MCA, and velocity measurements are automatically acquired by using an in-house flow tool.

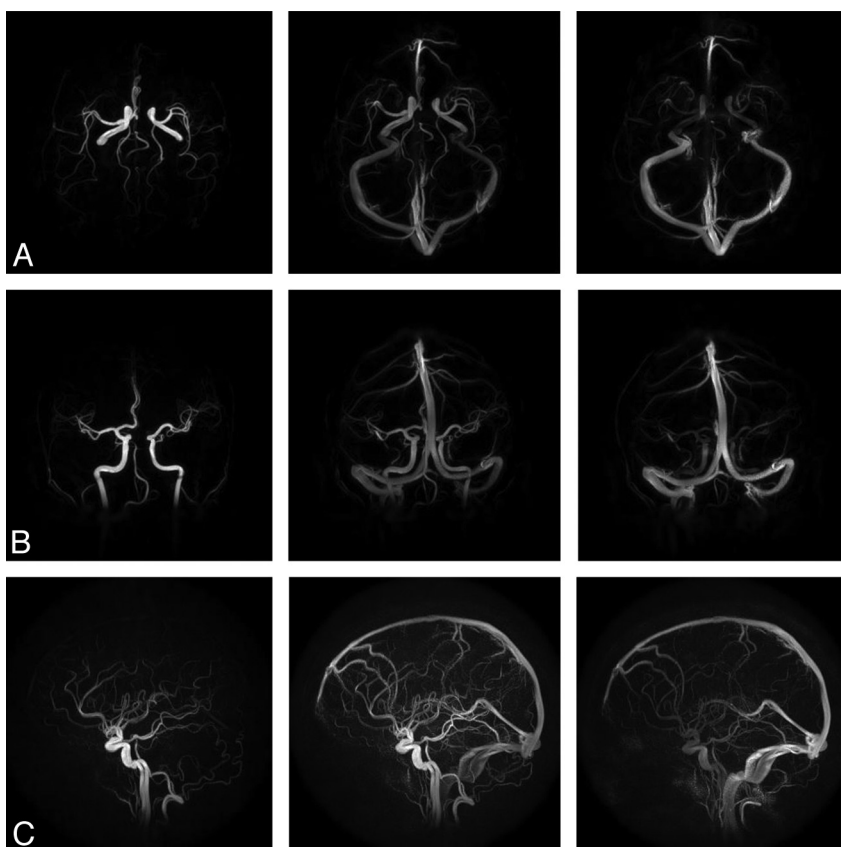


Fig 3. Representative images from a 60-frame time-series of the whole brain acquired by using PC HYPRFlow showing the early arterial, mixed, and venous phases: axial (A), coronal (B), and sagittal (C).

cycle was calculated for each volunteer. The maximum velocity over the cardiac cycle was designated as the peak systolic velocity, and the minimum velocity was designated as the minimum diastolic velocity. This process was repeated for data from the 2D-PC acquisition.

TCD Protocol

TCD imaging was performed in the MCAs bilaterally by using an Acuson-Sequoia sonography scanner (Siemens, Malvern, Pennsylvania) and a 4V1 MHz vector transducer. Depths for MCA interrogation were retrieved from the subjects' MRAs and given to the sonographer. The sonographer would attempt to replicate the depths when obtaining spectral Doppler signals. Color and spectral Doppler images were obtained via the transtemporal window. Once spectral Doppler images were obtained, mean, peak systolic, and end diastolic velocities were recorded. Three velocity measurements were obtained in each MCA.

Statistical Methods

Correlations were acquired between PC-VIPR and TCD and PC-VIPR and 2D-PC. Bland-Altman plots were generated comparing PC-VIPR and TCD and PC-VIPR and 2D-PC, and the bias and limits of agreement were calculated for each Bland-Altman plot. Statistics were calculated by using Excel 2007 (Microsoft, Bothell, Washington). The Pearson r was used for correlation analysis, and a P value $< .05$ for the correlation coefficient was considered statistically significant.

Results

Figure 3A–C shows axial, coronal, and sagittal whole-brain images acquired during the first pass of the contrast bolus by using PC HYPRFlow in the early arterial, mixed, and venous phases. Figure 4A, shows a velocity vector plot of the carotid terminus and the MCA and Figure 4B is a cross-section of the

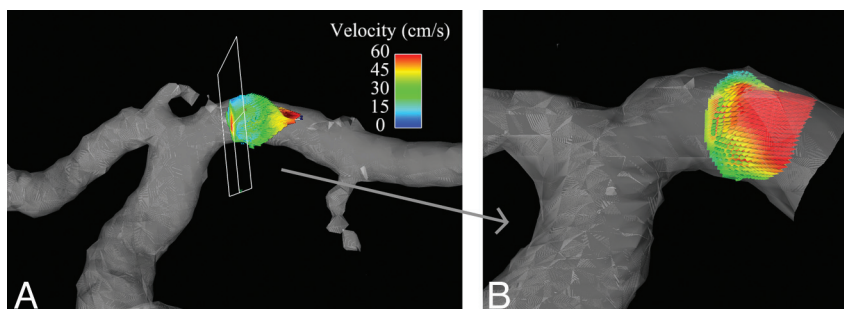


Fig 4. A, Segmentation of the carotid terminus showing velocity vectors in the MCA. B, Enlargement of a cross-section of the M1 segment of the MCA showing parabolic distribution of velocities in the MCA.

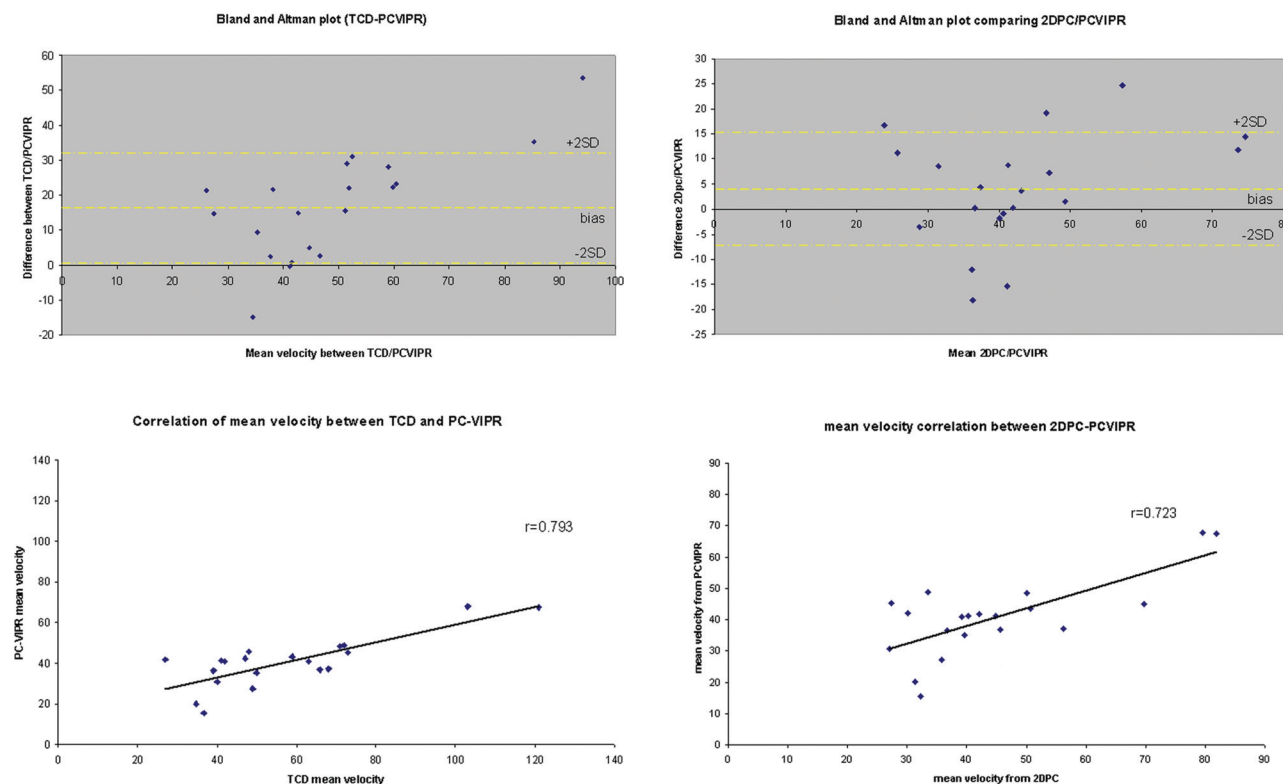


Fig 5. Top left: Bland-Altman plot of PC-VIPR compared with TCD. Top right: Bland-Altman plot of PC-VIPR compared with 2D-PC. Bottom left: Correlation plot of PC-VIPR with TCD. Bottom right: Correlation plot of PC-VIPR with 2D-PC.

MCA showing velocity vectors. Both plots show the parabolic distribution of velocities. The mean velocity (\pm SD) measured by sonography in the left and right MCAs of all volunteers ($n = 20$) was 57.54 ± 29.30 cm/s, peak systolic velocity was 85.21 ± 30.78 cm/s, and diastolic velocity was 41.42 ± 17.47 cm/s. Mean velocity measured by 2D-PC was 44.69 ± 16.09 cm/s, peak systolic was 64.59 ± 19.91 cm/s, peak diastolic was 29.79 ± 10.98 cm/s, and mean velocity measured by PC-VIPR was 43.17 ± 10.49 cm/s. Peak systolic was 58.39 ± 10.86 cm/s, and peak diastolic was 31.32 ± 12.00 cm/s. Bland-Altman analysis of PC-VIPR compared with TCD showed 17 of 20 points within 2 SDs, with a bias of 16.9 and 2 SD limits of agreement of 1.6 and 32, which is consistent with the values found in the literature showing that mean velocities acquired with PC-MRA are approximately 30% lower than those acquired by using TCD.²⁰⁻²⁴ Bland-Altman analysis of PC-VIPR compared with 2D-PC showed 14 of 20 points within 2 SDs,

with a bias of 4.05 and 2 SD limits of agreement of -7.15 and 15.2 . PC-VIPR and TCD were well correlated, with $r = 0.793$. PC-VIPR and 2D-PC showed a correlation of $r = 0.723$. P values of both correlations were $<.001$. Figure 5 shows the Bland-Altman and correlation plots between PC-VIPR and TCD (top) and PC-VIPR and 2D-PC (bottom).

Discussion

Velocity measurements are clinically useful both alone and in conjunction with vessel morphology and derivative measurements in identifying the extent and clinical impact of stenoses.⁸ The time-series, velocity measurements, and velocity derivatives acquired by using PC HYPRFlow demonstrate that this approach is an attractive alternative to other time-resolved and PC-MRA methods. We have previously shown that time-resolved CE PC HYPRFlow provides whole-brain images of diagnostic quality for the assessment of vascular

Imaging parameters							
Scan	TR/TE (ms)	α	Bandwidth (kHz)	Scanning Time (s)	VENC (cm/s)	FOV (mm)	Resolution (mm ³)
CE-VIPR	3.1/0.4	20	125	60		260 × 260 × 260	2 × 2 × 2
PC-VIPR	8.2/2.8	20	83.3	300	80–120	220 × 220 × 220	0.68 × 0.68 × 0.68
2D-PC	7.4/4.2	10	125	180	80–120	240 × 192	0.63 × 0.63 × 8

structures as small as 2.0 mm in diameter.⁹ In this study, we demonstrated that the PC-VIPR component of PC HYPRFlow is capable of velocity measurements consistent with 2 reference standards, product 2D-PC-MRA and TCD.

TCD is commonly used for velocity measurements, but the thickness of the skull makes it challenging to obtain measurements from many intracranial blood vessels. While the temporal bone window allows the proximal MCA and parts of the internal carotid artery to be visualized, other important segments are difficult or impossible to measure by using TCD. In this study, we showed that PC-VIPR provides velocity measurements from the MCA that are consistent with other PC-MRA/TCD correlations in the literature.^{20–24} In general, due to temporal averaging, velocity measurements by using PC-MRA are 30% less than those of TCD because TCD essentially has real-time temporal resolution, making it easier to sample the maximum-velocity near-peak systole. PC-MRA accuracy is influenced by several factors that have the potential to report lower maximum velocities. First, PC-MRA is a gated technique. If the peak velocity position and amplitude are shifted from heartbeat to heartbeat, PC-MRA will capture an average velocity over multiple heartbeats. Also, PC-MRA assumes a single velocity/voxel model. Thus, disturbed flow and resolution effects limit the detection of peak velocities. Finally, the temporal resolution of PC-MRA is substantially lower than that in sonography, causing PC-MR imaging to temporally blur and lower measured peak velocities.^{23,24} Nonetheless, the velocities were well-correlated and can easily be used to compare baseline velocities from those seen in pathologic conditions. The values acquired by using a whole-brain PC-VIPR acquisition were also similar to those acquired by using product 2D-PC-MRA in a much smaller FOV. PC-VIPR is capable of acquiring velocity measurements from the whole brain without the limitations of sonography, while also providing whole-brain 4D angiograms showing morphology and a time-series.

Emerging data indicate a link between abnormal WSS and the development and progression of both atherosclerotic plaques^{25,26} and saccular and fusiform cerebral aneurysms.^{8,27} Previous efforts to calculate WSS with PC-MRA have had limited success because of lack of sufficient spatial resolution within clinically useful scanning times,²⁸ boundary-zone localization, and aliasing, especially in areas of stenosis. PC-VIPR acquires whole-brain angiograms with high spatial resolution ($0.68 \times 0.68 \times 0.68$ mm³), which provides 8–12 pixels within the MCA. Using automated spline interpolation,^{28,29} we were able to visualize the boundary zone and acquire automated WSS calculations by using velocity data from PC-VIPR. We have also introduced a 5-point velocity-encoding tool that is capable of decreasing velocity aliasing.³⁰ This helps acquire velocity measurements in areas of high velocity, such as stenoses.

Limitations

While PC HYPRFlow has high spatial resolution compared with techniques in current clinical use, the spatial resolution is still relatively low compared with that typically used to calculate WSS in computational fluid dynamics³¹ and digital subtraction angiography in the acquisition of morphologic angiograms. At this time, this limitation restricts the vessels that can be imaged with diagnostic quality with PC HYPRFlow to medium- and large-sized vessels. However, with the advent of 32-channel head coils, higher spatial resolution will be achievable, allowing smaller vessels to be imaged and velocity and WSS to be calculated in smaller vessels as well.³² Similarly, these changes can also improve temporal resolution, allowing peak systolic velocity to be better detected. Patient motion is an issue, but we have implemented image registration to correct this problem.

Conclusions

PC HYPRFlow is a comprehensive technique that acquires both morphologic images of diagnostic quality and velocity data in 5–6 minutes. The PC-VIPR component of PC HYPRFlow provides velocity measurements consistent with 2D-PC and TCD in medium and large intracranial vessels.

Acknowledgments

We thank the following individuals for their important contributions to this project: Sara Baker, MEd, RT, and Carol Mitchell, PhD, for supervision and performance of the TCD studies; Sara Pladziewicz, RT, and Kelli Hellenbrand, RT, for performance of the PC HYPRFlow examinations; and Kari Pulfer, RT, for subject recruitment.

References

1. Lotz J, Doker R, Noeske R, et al. **In vitro validation of phase-contrast flow measurements at 3 T in comparison to 1.5 T: precision, accuracy, and signal-to-noise ratios.** *J Magn Reson Imaging* 2005;21:604–10
2. Korosec F, Turski P. **Velocity and volume flow rate measurements using phase contrast magnetic resonance imaging.** *International Journal of Neuroradiology* 1997;3: 293–318
3. Baledent O, Fin L, Khuoy L, et al. **Brain hydrodynamics study by phase-contrast magnetic resonance imaging and transcranial color Doppler.** *J Magn Reson Imaging* 2006;24:995–1004
4. Yamashita S, Isoda H, Hirano M, et al. **Visualization of hemodynamics in intracranial arteries using time-resolved three-dimensional phase-contrast MRI.** *J Magn Reson Imaging* 2007;25:473–78
5. Markl M, Hennig J. **Phase contrast MRI with improved temporal resolution by view sharing: k-space related velocity mapping properties.** *J Magn Reson Imaging* 2001;19:669–76
6. Sodickson DK, Manning WJ. **Simultaneous acquisition of spatial harmonics (SMASH): fast imaging with radiofrequency coil arrays.** *Magn Reson Med* 1997;38:591–603
7. Griswold MA, Jakob PM, Heidemann RM, et al. **Generalized autocalibrating partially parallel acquisitions (GRAPPA).** *Magn Reson Med* 2002;47:1202–10
8. Hope TA, Hope MD, Purcell DD, et al. **Evaluation of intracranial stenoses and aneurysms with accelerated 4D flow.** *J Magn Reson Imaging* 2010;28:41–46. Epub 2009 Jul 3
9. Wu Y, Chang W, Johnson K, et al. **Fast whole brain 4D contrast enhanced MR**

- angiography with velocity encoding using undersampled radial acquisition and highly constrained projection reconstruction: image quality assessment in volunteer subjects. *AJNR Am J Neuroradiol*, 2010 Nov 24. [Epub ahead of print]
10. Peters DC, Korosec FR, Grist TM, et al. Undersampled projection reconstruction applied to MR angiography. *Magn Reson Med* 2000;43:91–101
 11. Mistretta CA. Undersampled radial MR acquisition and highly constrained back projection (HYPR) reconstruction: potential medical imaging applications in the post-Nyquist era. *J Magn Reson Imaging* 2009;29:501–16
 12. Velikina JV, Johnson KM, Wu Y, et al. PC HYPR flow: a technique for rapid imaging of contrast dynamics. *J Magn Reson Imaging* 2010;31:447–56
 13. Johnson K, Lum D, Turski P, et al. Improved 3D phase contrast MRI with off-resonance corrected dual echo VIPR. *Magn Reson Med* 2008;60:1329–36
 14. Mistretta CA, Wieben O, Velikina J, et al. Highly constrained backprojection for time-resolved MRI. *Magn Reson Med* 2006;55:30–40
 15. Gu T, Korosec FR, Block WF, et al. PC VIPR: a high-speed 3D phase-contrast method for flow quantification and high-resolution angiography. *AJNR Am J Neuroradiol* 2005;26:743–49
 16. Moftakhar R, Aagaard-Kienitz B, Johnson K, et al. Noninvasive measurement of intra-aneurysmal pressure and flow pattern using phase contrast with vastly undersampled isotropic projection imaging. *AJNR Am J Neuroradiol* 2007;28:1710–14
 17. Turk AS, Johnson KM, Lum D, et al. Physiologic and anatomic assessment of a canine carotid artery stenosis model utilizing phase contrast with vastly undersampled isotropic projection imaging. *AJNR Am J Neuroradiol* 2007;28:111–15
 18. Brodsky EK, Lu A, Thornton FJ, et al. Using multiple half-echoes to improve sampling efficiency and fat suppression in time-resolved MRA. In: *Proceedings of the 11th Annual Meeting of the International Society for Magnetic Resonance in Medicine*, Toronto, Ontario, Canada. July 10–16, 2003:74
 19. Nett E, Johnson K, Francois C, et al. Analysis platform for hemodynamic function in congenital heart disease. *J Cardiovasc Magn Reson* 2009;11(suppl 1):P212
 20. Wetzel S, Meckel S, Frydrychowicz A., et al. In vivo assessment and visualization of intracranial arterial hemodynamics with flow-sensitized 4D MR imaging at 3T. *AJNR Am J Neuroradiol* 2004;28:433–38
 21. Lotz J, Meier C, Leppert A, et al. Cardiovascular flow measurement with phase-contrast MR imaging: basic facts and implementation. *Radiographics* 2002;22:651–71
 22. Oktar SO, Yücel C, Karaosmanoglu D, et al. Blood-flow volume quantification in internal carotid and vertebral arteries: comparison of 3 different ultrasound techniques with phase-contrast MR imaging. *AJNR Am J Neuroradiol* 2006;27:363–69
 23. Stadlbauer A, van der Riet W, Globits S, et al. Accelerated phase-contrast MR imaging: comparison of k-t BLAST with SENSE and Doppler ultrasound for velocity and flow measurements in the aorta. *J Magn Reson Imaging* 2009;29:817–24
 24. Seitz J, Strotzer M, Wild T, et al. Quantification of blood flow in the carotid arteries: comparison of Doppler ultrasound and three different phase-contrast magnetic resonance imaging sequences. *Invest Radiol* 2001;36:642–47
 25. Malek A, Alper S, Izumo S. Hemodynamic shear stress and its role in atherosclerosis. *JAMA* 1999;282:2035–42
 26. Cunningham K, Gotlieb A. The role of shear stress in the pathogenesis of atherosclerosis. *Lab Invest* 2005;85:9–23
 27. Hoi Y, Meng H, Woodward SH, et al. Effects of arterial geometry on aneurysm growth: three-dimensional computational fluid dynamics study. *J Neurosurg* 2004;101:676–81
 28. Stalder AF, Russe MF, Frydrychowicz A, et al. Quantitative 2D and 3D phase contrast MRI: optimized analysis of blood flow and vessel wall parameters. *Magn Reson Med* 2008;60:1218–31
 29. Chang W, Wentland A, Johnson K, et al. Calculation of wall shear stress in the middle cerebral arteries of healthy volunteers using PC-VIPR, a fast whole-brain undersampled 3D-radial PC-MRA technique. In: *Proceedings of the 18th Annual Meeting of the International Society of Magnetic Resonance in Medicine*, Stockholm, Sweden; May 1–7, 2010
 30. Johnson K, Markl M. Improved SNR in phase contrast velocimetry with five-point balanced flow encoding. *Magn Reson Med* 2010;63:349–55
 31. Wood N, Weston S, Kilner P, et al. Combined MR imaging and CFD simulation of flow in the human descending aorta. *J Magn Reson Imaging* 2001;13:699–713
 32. van Zijl P. 32-channel coil boosts 3.0T neuroimaging at Kennedy Krieger. *Field Strength* 2009;9:14–18