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Differentiating Atypical Hemangiomas and Metastatic Vertebral Lesions: The Role of T1-Weighted Dynamic Contrast-Enhanced MRI

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ABSTRACT

BACKGROUND AND PURPOSE: Vertebral hemangiomas are benign vascular lesions that are almost always incidentally found in the spine. Their classic typical hyperintense appearance on T1- and T2-weighted MR images is diagnostic. Unfortunately, not all hemangiomas have the typical appearance, and they can mimic metastases on routine MR imaging. These are generally referred to as atypical hemangiomas and can result in misdiagnosis and ultimately additional imaging, biopsy, and unnecessary costs. Our objective was to assess the utility of dynamic contrast-enhanced MR imaging perfusion in distinguishing vertebral atypical hemangiomas and malignant vertebral metastases. We hypothesized that permeability and vascular density will be increased in metastases compared with atypical hemangiomas.

MATERIALS AND METHODS: Consecutive patients from 2011 to 2015 with confirmed diagnoses of atypical hemangiomas and spinal metastases from breast and lung carcinomas with available dynamic contrast-enhanced MR imaging were analyzed. Time-intensity curves were qualitatively compared among the groups. Perfusion parameters, plasma volume, and permeability constant were quantified using an extended Tofts 2-compartment pharmacokinetic model. Statistical significance was tested using the Mann-Whitney *U* test.

RESULTS: Qualitative inspection of dynamic contrast-enhanced MR imaging time-intensity curves demonstrated differences in signal intensity and morphology between metastases and atypical hemangiomas. Quantitative analysis of plasma volume and permeability constant perfusion parameters showed significantly higher values in metastatic lesions compared with atypical hemangiomas ($P < .001$).

CONCLUSIONS: Our data demonstrate that plasma volume and permeability constant perfusion parameters and qualitative inspection of contrast-enhancement curves can be used to differentiate atypical hemangiomas from vertebral metastatic lesions. This work highlights the benefits of adding perfusion maps to conventional sequences to improve diagnostic accuracy.

ABBREVIATIONS: DCE = dynamic contrast-enhanced; k^{trans} = permeability constant; VH = vertebral hemangioma; V_p = plasma volume

Vertebral hemangiomas (VHs) are the most common benign tumors of the spine. They compose 28% of all skeletal hemangiomas, and the thoracic spine is the most frequent location.¹ VHs are often an incidental finding, having been found in 11% of spines in a large study of postmortem examinations.² VHs are

more frequently found in women, especially in the fourth-to-sixth decades of life.³ These lesions can affect a segment or the entirety of the vertebral body, and they are multiple in roughly one-third of patients.⁴ Most are stable and asymptomatic, but they can become clinically relevant with atypical imaging characteristics when establishing the presence of metastatic disease or when dealing with an aggressive/symptomatic hemangioma, which can induce pain, fractures, and neurologic manifestations due to spinal cord compression.⁵

Histologically, VHs are characterized by vascular spaces lined with endothelial cells of mature thin-walled blood vessels and sinuses lined by flattened or attenuated endothelium. Vessels are scattered, surrounded by a fatty matrix and vertically oriented trabeculae of bone, probably causing resorption of underlying

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bone and thickening of the remaining trabeculae.³ The characteristic radiologic appearance is defined by its histologic architecture demonstrating a parallel striated pattern, “corduroy cloth,” on plain film and on sagittal or coronal CT and a spotted appearance, “polka dot,” on axial CT.^{3,6} The MR imaging appearance is also influenced by the proportion of histologic components. Postmortem specimens of VHs have been examined with MR imaging and correlated histologically, demonstrating that the signal intensity on T1- and T2-weighted imaging is associated with the fraction of the lesion occupied by adipocytes, vessels, and edema.⁷ Typical VHs are hyperintense on T1 and T2, especially on FSE sequences because of their fatty stroma and vascular components, demonstrating variable enhancement, lower in lesions with a larger fatty content.³ On the other hand, atypical VHs have low fat content and high vascularity, displaying an iso-/hypointense signal on T1- and hyperintense signal on T2-weighted images with elevated contrast enhancement. Also, some atypical VHs are more likely to show aggressive behavior when there is an increased vascular component and less fatty stroma. Cortical erosion, extradural soft tissue, expansion to the posterior elements, and even invasion of the spinal canal, are radiologic signs of aggressiveness.³ While these incidentally found lesions are benign, their appearance on routine STIR and T1- and T2-weighted MR images often mimics that of primary bone malignancies and metastatic lesions.⁸ Therefore, the ability to distinguish these commonly encountered lesions and vertebral malignancies has a direct clinical application in patient management, particularly in a patient with known malignancy.

Dynamic contrast-enhanced (DCE) MR imaging perfusion allows obtaining physiologic information about the microvascular environment of the lesion by applying a pharmacokinetic model procuring quantitative parameters such as plasma volume (V_p), representing the vascular density of the lesion of interest, and permeability constant (K^{trans}), which provides information about blood exchange between the vascular and interstitial compartments. These quantitative parameters have demonstrated their value in detecting the differences in the microvascular environment among metastatic lesions before and after treatment,⁹ benign and pathologic fractures,¹⁰ and hypovascular and hypervascular lesions.^{11,12} Vertebral metastases demonstrate very different histologic patterns, depending on the primary tumor. There is, however, a common feature in all of them: neoangiogenesis. The microenvironment of the metastasis induces secretion of proangiogenic growth factors that promote the development of new fragile and hyperpermeable vessels. The purpose of our study was to assess the utility of DCE MR imaging perfusion in distinguishing vertebral atypical hemangiomas and vertebral metastases, which otherwise can be undistinguishable in routine spine MR imaging. We hypothesized that permeability and vascular density would be increased in metastases because they are associated with a greater concentration of new aberrant and fragile vessels compared with hemangiomas.

MATERIALS AND METHODS

Our study was compliant with the Health Insurance Portability and Accountability Act and was approved by the institutional review board of Memorial Sloan Kettering Cancer Center. The need for informed consent was waived.

Atypical VH Lesions

A hospital data base was reviewed from January 2012 to June 2015. The query yielded 54 consecutive patients with the radiologic diagnosis of atypical VHs. The initial selection was based on the radiologic appearance (iso-/hypointensity on T1 and hyperintensity on STIR) and proved histology (if available). Cases without histology were included on the basis of the following criteria: the assessment of lesion stability after 1 year, negative PET/CT scan findings, and/or presence of the characteristic trabecular appearance on CT. Exclusion criteria from DCE MR imaging analysis comprised the following: lesions that did not meet the stability criteria after 1 year, a history of radiation therapy, or histology positive for malignancy. These selection criteria yielded 34 lesions present in 28 patients.

Metastatic Lesions

Consecutive patients who underwent spine needle biopsy during 2011–2013 were evaluated for vertebral metastatic lesions and classified on the basis of their primary carcinoma origin. Consecutive patients with primary carcinomas of breast ($n = 28$) and lung ($n = 14$) with available DCE MR imaging data were included for 42 metastatic lesions. Patients who had undergone radiation therapy, an operation, and/or kyphoplasty in the lesion of interest were excluded.

Data Acquisition

MR imaging sequences were acquired as a part of standard clinical protocol with a 1.5T or 3T scanner (Optima 450w or Discovery MR750w; GE Healthcare, Milwaukee, Wisconsin) using an 8-channel cervical-thoracic-lumbar surface coil. All patients underwent routine MR imaging, including sagittal T1-weighted fast spin-echo (FOV, 32–36 cm; slice thickness, 3 mm; TR, 400–650 ms; TE, 8.4 ms; flip angle, 160°; in-plane resolution, $1.4 \times 1.4 \text{ mm}^2$), T2-weighted FSE (FOV, 32–36 cm; slice thickness, 3 mm; TR, 3500–4000 ms; TE, 110 ms; flip angle, 160°; in-plane resolution, $1.4 \times 1.4 \text{ mm}^2$), and sagittal STIR FSE (FOV, 32–36 cm; slice thickness, 3 mm; TR, 3500–6000 ms; TE, 10 ms; flip angle, 160°; in-plane resolution, $1.4 \times 1.4 \text{ mm}^2$).

For DCE MR imaging, a bolus of Gd-DTPA was administered by a power injector at 0.1 mmol/kg of body weight and a rate of 2–3 mL/s. The kinetic enhancement of tissue during and after injection of Gd-DTPA was obtained before, during, and after contrast injection using a 3D T1-weighted fast-spoiled gradient recalled-echo sequence (TR, 4–5 ms; TE, 1–2 ms; slice thickness, 5 mm; flip angle, 25°; FOV, 32 cm; temporal resolution, 6–7 seconds) and consisted of 10–12 images in the sagittal plane. The duration of the DCE sequence was 200–240 seconds. Sagittal and axial T1-weighted post-Gd-DTPA MR images were acquired after DCE MR imaging.

Data Processing and Analysis

Data processing and analysis were performed using dynamic image-processing software (nordicICE; NordicNeuroLab, Bergen, Norway). Preprocessing steps integrated background noise subtraction, spatial and temporal smoothing, and detection of the arterial input function from the aorta. ROIs were manually drawn and confirmed by an experienced neuroradiologist who was blinded to the diagnosis on perfusion maps. For accurate mea-

surement of perfusion parameters, vessels, venous structures, and vertebral body endplates were carefully excluded from the ROIs. Anatomic images that matched the DCE MR images were used in ROI placements. Time-intensity curves in the ROI were then obtained. Voxel-by-voxel estimates of quantitative perfusion parameters, including vascular permeability and plasma volume, were determined on the basis of the extended Tofts 2-compartment pharmacokinetic model.¹³ For lesions with multiple slices, these perfusion values were determined for each slice and the maximum values of V_p and K^{trans} were obtained in the ROIs and were used for statistical analysis.

Imaging Analysis

Time-intensity curve morphologies were qualitatively analyzed and compared among the groups (atypical VHs versus metastatic lesions). The time-intensity curves were classified into 5 types according to Chen et al¹⁴: type A (a nearly flat time-intensity curve), type B (a slow-inclination curve), type C (rapid wash-in, followed by a plateau), type D (rapid wash-in followed by a wash-out phase), and type E (initial rapid wash-in followed by a second slowly rising phase).

For quantitative parameters, including K^{trans} and V_p , ROI values were determined for each slice of the lesion and the maximum values of V_p and K^{trans} were used for the comparison.

Statistical Analysis

A Mann-Whitney *U* test at a significance level of $P < .01$ was performed to determine the difference in the DCE MR imaging perfusion parameters, V_p and K^{trans} , between the vertebral metastases and atypical hemangiomas.

RESULTS

A sharp difference in both morphology and signal intensity is observed when comparing time-intensity curves (Fig 1). Metastatic lesions show enhancement curves resembling type D curve morphology as described by Chen et al.¹⁴ These exhibit a sharp rise (slope) and higher peak signal intensity, followed by a faster washout phase. Most atypical hemangiomas have a minimal and delayed enhancement and fall within a narrow range, except for the 4 curves highlighted in cyan in Fig 2A, which deviate significantly from this range. These 4 lesions met the stability inclusion criteria and therefore were not excluded from the analysis. Although vertebral vessels were always carefully excluded from the ROIs, some of these lesions have considerable extension through the entire vertebral body and could represent rare cases in which atypical hemangiomas display an aggressive behavior and substantial vascularity and vertebral body invasion occur. If we evaluated the curve average intensity excluding these 4 cases (Fig 2B), 88% of the atypical hemangioma curves analyzed would show a characteristic pattern with minimum and late enhancement curves with no evident washout in contrast to metastases, which display a rapid wash-in phase, higher peak, and clear washout (Fig 2C).

Quantitative analysis demonstrates higher perfusion values (V_p and K^{trans}) of metastatic lesions than atypical hemangiomas ($P < .01$), despite an almost identical appearance on T1 (Figs 3 and 4). V_p values demonstrated the greatest difference and mini-

mal overlap between atypical vertebral hemangiomas and metastatic lesions, being the best biomarker. No significant differences were found when comparing lung and breast metastases ($P > .3$).

DISCUSSION

We compared 34 atypical hemangiomas and 42 metastatic vertebral lesions and found that DCE MR perfusion assessment of the TI curves and V_p and K^{trans} parameters demonstrated higher values in vertebral metastases compared with atypical vertebral hemangiomas. V_p was considered the best parameter to differentiate the 2 groups.

Noninvasive imaging biomarkers can be of paramount importance to help distinguish atypical VHs and metastatic vertebral lesions, especially when atypical VHs can mimic the pattern observed for primary malignant and metastatic lesions. Currently, long-term stability and the classic radiologic appearance are the imaging tools available to confirm the diagnosis. However, the vertical trabecular appearance has been reported to be more difficult to visualize in atypical hemangiomas, making the diagnosis even more challenging.⁸ Furthermore, although rare, VHs display “aggressive” behavior that can manifest as pain and radiculopathies when involvement of the entire vertebral body and compression of the spinal cord and nerve roots occur. These can be easily mistaken for malignancies and may result in additional diagnostic imaging, biopsy, and, in some cases, an operation. In addition, atypical VHs have been identified concurrent with metastatic disease from primary malignancy such as colon adenocarcinoma¹⁵ and thyroid cancer.¹⁶ Consequently, their accurate identification in these cases poses a major challenge with a large impact on patient staging and management.

In the past decade, our tools to identify these lesions have been limited. Effort has been made to differentiate hemangiomas and malignant lesions with the use of diffusion-weighted imaging and apparent diffusion coefficient calculations.¹⁷ Quantitative chemical shift MR imaging has also been used, and a proportional change in signal intensity on in-phase compared with out-of-phase images showed a decrease in signal intensity in benign lesions compared with metastatic lesions.¹⁸ However, no robust method has been established to differentiate atypical hemangiomas and metastatic spine lesions.

Our study takes advantage of spine DCE MR imaging perfusion as a noninvasive method of obtaining quantitative parameters representing the physiology of the microvascular environment of each lesion. Except for the aforementioned 4 cases, atypical hemangioma time-intensity curves had a minimal and delayed enhancement, with no evident washout in contrast to metastases, which display a rapid wash-in phase, higher peak, and clear washout, a common indicator of malignancy. In addition to the benign appearance of the curves, quantitative analysis of the perfusion parameters V_p and K^{trans} also demonstrated significantly lower perfusion values in atypical hemangiomas compared with metastatic lesions, despite an almost identical appearance on T1-weighted sequences.

Our findings reflect the physiology and histologic structure of atypical vertebral hemangiomas, less fat and greater vascular content. Most hemangiomas in our study showed low plasma volume and permeability. Only 4 cases demonstrated higher V_p values,

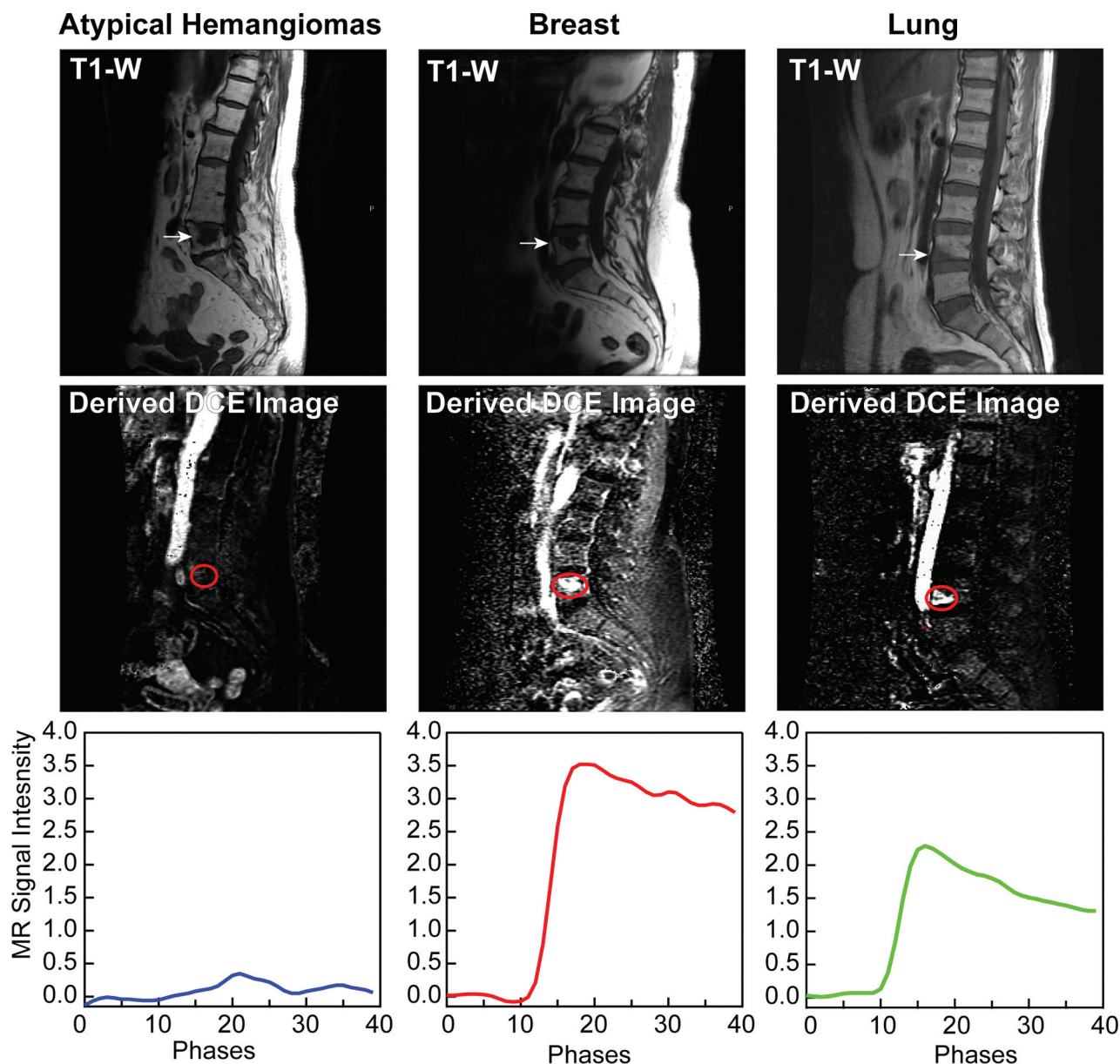


FIG 1. Representative sagittal T1-weighted and dynamic images derived from DCE MR imaging for atypical hemangiomas and spinal lesions originating from primary breast and lung carcinomas. The lower panel corresponds to the MR imaging signal enhancement curve as a function of phases (time) obtained for each representative lesion shown.

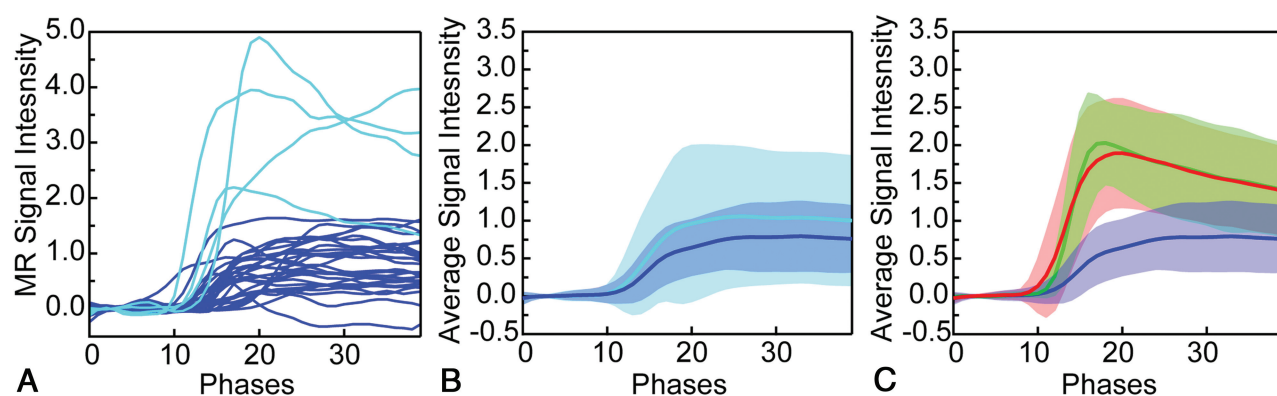


FIG 2. A, Enhancement curve for all 34 atypical hemangiomas. Curves highlighted in cyan show the 4 cases with elevated enhancement. B, Average enhancement curves for all atypical hemangiomas (cyan) excluding atypical hemangiomas with elevated enhancement (blue). C, Average enhancement curves for all atypical hemangiomas excluding enhancement curve outliers (blue) compared with breast (red) and lung (green) metastases.

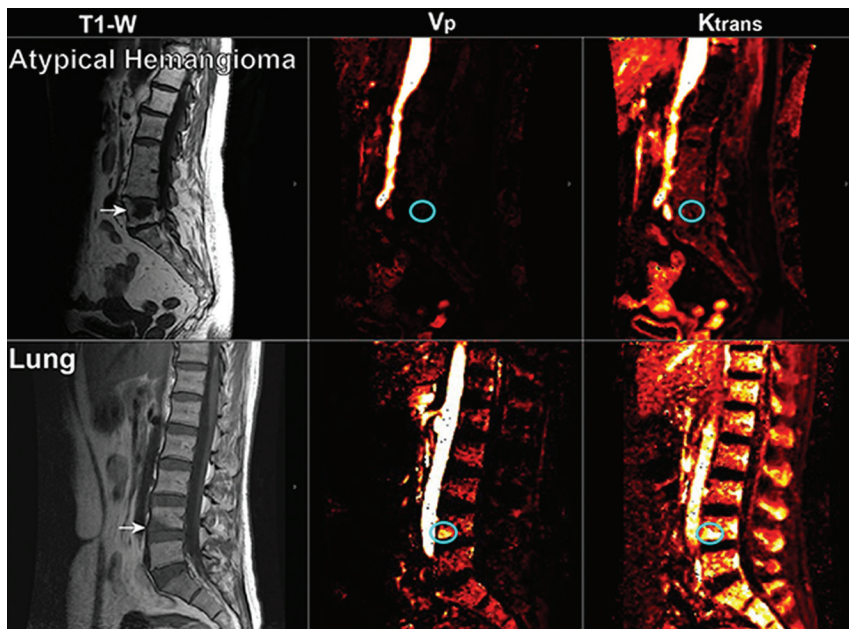


FIG 3. Representative sagittal T1-weighted imaging and the corresponding perfusion maps for V_p and K^{trans} parameters for atypical hemangiomas and metastasis from lung carcinoma. Arrows indicate the level of the lesion in T1WI, and the cyan circle highlights the region on V_p and K^{trans} maps where the lesion is located.

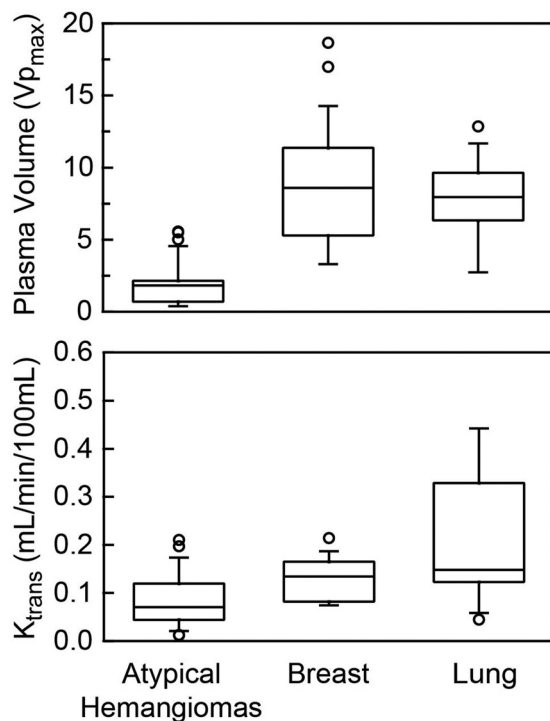


FIG 4. V_p and K^{trans} parameters obtained for atypical hemangiomas and metastatic lesions from breast and lung carcinoma. Metastases show significantly higher values ($P < .05$) for both V_p and K^{trans} compared with atypical vertebral hemangiomas. Note that the 4 outlier values representing aggressive hemangiomas account for the higher V_p values in the atypical hemangioma group that demonstrate minimal overlap with the metastatic group and remain low compared with other metastases.

which overlap those of the metastatic lesions. These 4 cases probably represent aggressive or compressive vertebral hemangiomas, which exhibit a higher degree of vascularization and an expansile soft-tissue component.¹⁹ This subgroup is associated with some features that help distinguish it from atypical quiescent hemangiomas, such as involvement of the entire vertebral body, extension into the neural arch, cortical expansion, midthoracic location, irregular honeycomb pattern, and soft-tissue mass, according to Laredo et al.¹⁹ In fact, 3 of the 4 lesions were expanding into the posterior vertebral elements, and one demonstrated ventral epidural disease. The remaining lesion was a small well-demarcated hemangioma confined to the vertebral body. However, the 4 cases demonstrated lower values of K^{trans} (0.08, 0.08, 0.09, and 0.11) than those seen on metastases (K^{trans} mean, 0.15), in keeping with the expected low permeability due to a theoretically preserved endothelium in these lesions.

As with Laredo et al,¹⁹ we suggest that DCE MR imaging perfusion can be a useful tool for differentiating quiescent atypical VHs that represent localized, relatively inactive angiomatous dysmorphies from aggressive atypical VHs that show extensive, active angiomatous tumors that can compress the spinal cord and become symptomatic.¹⁹ When there is an abnormally elevated V_p , K^{trans} can be helpful in demonstrating preservation of permeability, suggesting a benign etiology.

Our study has several limitations. First, it is a retrospective study with the possibility of selection bias. Second, there was no pathologic confirmation for most of the atypical hemangiomas; however, all these lesions were stable after 1 year, had negative findings on PET/CT, and/or had the characteristic trabecular appearance on CT. Third, the manual ROI selection, though a standard method of analyzing perfusion data, is an operator-dependent technique associated with potential interobserver and intraobserver variability. However, having 1 single trained operator performing the measurements limits the potential variation. Fourth, there is limited representation of other malignancies in the metastatic group that could have demonstrated different perfusion patterns. On the other hand, lung and breast are by far the most representative primary malignancies, accounting for 31% and 24% of all sources of spinal metastatic disease. Despite these limitations, this is the first study of its kind to compare atypical VHs and vertebral metastases using DCE MR imaging, to our knowledge.

CONCLUSIONS

Our data demonstrate that qualitative inspection of contrast-enhancement curves and quantitative analysis of V_p and K^{trans} perfusion parameters can be used to differentiate atypical hemangi-

omas from vertebral metastatic lesions. The ability of DCE MR imaging to noninvasively characterize tumor vascularity has important clinical implications, which could lead to changes in patient management, reducing biopsies, hospital stay, additional imaging, and patient anxiety.

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