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MR Imaging for Differentiating Contrast Staining from Hemorrhagic Transformation after Endovascular Thrombectomy in Acute Ischemic Stroke: Phantom and Patient Study

S.-H. You, B. Kim, B.K. Kim, and S.-i. Suh



ABSTRACT

BACKGROUND AND PURPOSE: Early differentiation of contrast staining from hemorrhagic transformation in patients with acute ischemic stroke who have undergone endovascular treatment is critical in preventing the delayed administration of antiplatelet agents. We aimed to demonstrate the usefulness of an immediate postinterventional DWI protocol including B_0 and gradient recalled-echo sequences to discriminate those 2 conditions through phantom and preliminary retrospective patient studies.

MATERIALS AND METHODS: On 3T MR imaging, the signal intensities of the phantom models consisting of iodinated contrast agents diluted with normal saline and arterial blood were compared using T1WI, T2WI, and gradient recalled-echo sequences. A total 17 patients (8 with hemorrhagic transformation and 9 with contrast staining; 8 men and 9 women; mean age, 72.00 ± 10.91 years; range, 52–90 years) who underwent mechanical thrombectomy for acute ischemic stroke and showed newly appearing hyperdense lesions on immediate (<24 hours) postinterventional nonenhanced CT scans were included in this study. Immediate postinterventional DWI of patients were compared.

RESULTS: In the phantom study, iodinated contrast agents diluted with normal saline showed minimal signal drop, while those diluted with arterial blood demonstrated dark signal intensity in the T2WI and gradient recalled-echo sequences. In the patient study, all hemorrhagic transformations and none of the contrast staining demonstrated dark or low signal (<gray matter) intensities similar to those of the vessel in the B_0 -DWI and gradient recalled-echo images.

CONCLUSIONS: According to our preliminary results, contrast staining might be differentiated from hemorrhagic transformation using an immediate postinterventional DWI protocol including gradient recalled-echo sequences. It might be possible to expedite establishment of postinterventional medical treatment strategy.

ABBREVIATIONS: CT_{FU} = postinterventional (24–72 hours) follow-up nonenhanced brain CT; CT_{imme} = postinterventional (<24 hours) nonenhanced brain CT; GRE = gradient recalled-echo; IODBL = iodinated contrast agents diluted with arterial blood; IODNS = iodinated contrast agents diluted with normal saline

After endovascular treatment in patients with acute ischemic stroke, newly developed parenchymal hyperdensity is frequently encountered in immediate postinterventional CT images (31%–61%).^{1–3} Although a large proportion (73%–79%) of the parenchymal hyperdensity represents contrast staining, the rest is associated with hemorrhagic transformation. During intra-arterial thrombolysis or thrombectomy, not only the underlying isch-

emic change but also the intra-arterial thrombolytics and mechanical injury could cause disruption of the blood-brain barrier. Additionally, a large number of concentrated iodinated contrast agents promote breakdown of the blood-brain barrier via chemical irritation.^{4,5} It is possible for contrast agents to escape from the vessels when the blood-brain barrier breaks down, but cellular components of the blood, such as red blood cells, cannot leak from the vessels. This phenomenon is called contrast staining, contrast enhancement, or contrast extravasation.^{3,5–7} It is not a risk factor for hemorrhagic transformation; therefore, the rapid introduction of antiplatelet agents is possible to prevent re-occlusion in patients with acute infarction.^{2,3} In contrast, if the basal lamina and the blood-brain barrier are degraded by more severe injury, hemorrhagic transformation may occur. Under such circumstances, antiplatelet agents should not be administered to prevent the progression of the hemorrhage. Therefore, early differentiation of contrast staining from hemorrhagic transforma-

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tion is critical to establish an optimal postinterventional treatment strategy using antiplatelet agents.

In principle, it is difficult to differentiate parenchymal hyperdensity resulting from contrast staining from hemorrhagic transformation on immediate postinterventional CT (<24 hours) due to the similar Hounsfield densities of the lesions.^{1,2,8} Although early diagnosis of hemorrhagic transformation after endovascular treatment is crucial, it may be differentiated from contrast staining only via follow-up CT (24–48 hours). In this study, we were interested in differentiating contrast staining from hemorrhagic transformation using DWI and gradient recalled-echo (GRE) imaging. The negative susceptibility and T2-shortening effect of iodinated contrast agents have been demonstrated in previous phantom and animal studies.⁹ However, no studies have compared the signal intensities of iodinated contrast agents diluted with normal saline (IODNS) representing contrast staining and those diluted with arterial blood (IODBL) representing hemorrhagic transformation. Additionally, the usefulness of the immediate postinterventional DWI protocol for differentiating contrast staining and hemorrhagic transformation has not yet been elucidated using patient data. The aim of the present study was to compare the MR signal intensities of iodinated contrast agents mixed with normal saline and arterial blood in a phantom model. We also aimed to validate the usefulness of an immediate postinterventional DWI protocol, including B_0 and GRE imaging to discriminate contrast staining and hemorrhagic transformation using retrospective patient imaging data.

MATERIALS AND METHODS

Phantom Model

Forty-two 5-mL cylindric plastic tubes were prepared for the phantom. The diameter and height of the tubes were 10 and 50 mm, respectively. The inner walls of the tubes were coated with heparin.

Thirty-five cells of the phantom were filled with 5 different kinds of nonionic iodinated contrast agents (Visipaque, iodoxanol, 320 I mg/mL, 2.5 I mol/L, iso-osmolar, GE Healthcare, Piscataway, New Jersey; Omnipaque, iohexol, 350 I mg/mL, 2.8 I mol/L, low-osmolar, GE Healthcare; Xenetix, iobitridol, 300 I mg/mL, 2.4 I mol/L, low-osmolar, Guerbet, Roissy, France; Iomeron, iomeprol, 300 I mg/mL, 2.4 mol/L, low-osmolar, Bracco, Milan, Italy; and Pamiray, iopamidol, 300 I mg/mL, 2.4 mol/L, low-osmolar, Dongkook Pharm, Seoul, Korea) diluted with normal saline (0.9% sodium chloride) at 7 different concentrations (0, 0.1, 0.4, 0.6, 1.2, 2, and 2.4 I mol/L). The remaining 7 cells were filled with one of the nonionic iodinated contrast agents (Visipaque) diluted with arterial blood at 7 different concentrations (0, 0.1, 0.4, 0.6, 1.2, 2, and 2.4 I mol/L). In a previous pilot study, the aforementioned 5 nonionic iodinated contrast agents showed the same tendency toward magnetic fields regardless of their different side chains. Therefore, we diluted a representative contrast agent with human arterial blood for the phantom of IODBL.

MR Imaging Acquisition and Analysis of Phantom

The phantom with IODNS and IODBL was scanned by a 3T MR imaging unit (Tim Trio; Siemens, Erlangen, Germany) using spin-echo acquisitions with T1WI (TR/TE, 500/10 ms), T2WI (TR/TE, 6000/115 ms), and GRE (TR/TE, 535/15 ms) sequences.

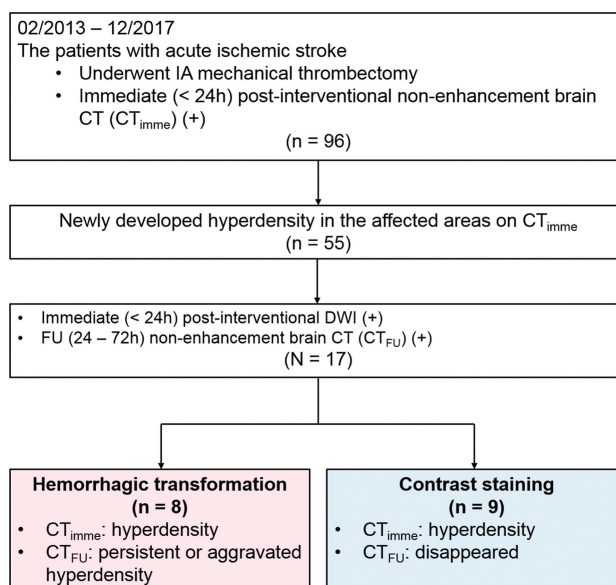


FIG 1. Study design.

The T1WI, T2WI, and GRE sequences were scanned in a visual analysis; then, another T2WI was performed after changing the TE (8.4–185 ms, TR fixed at 2500 ms, 1 single acquired FOV of 123 × 250 mm, and a matrix of 256 × 126) to measure the T2-relaxation time. All the blood-containing tubes were replaced with new tubes containing newly sampled arterial blood and the same concentration of iodinated contrast agents to maintain the same chemical status of hemoglobin. Finally, another T1WI was acquired after changing the TR (180–250 ms, TE fixed at 8.7 ms, 1 single acquired FOV of 123 × 250 mm, and a matrix of 256 × 126).

After reading the DICOM data from the MR imaging system, the T1- and T2-relaxation times for the phantom were calculated using a software for analyzing functional neuroimaging data.

Patients

This retrospective study was approved by the institutional review board of Korea University Anam Hospital. Informed consent was waived because of its retrospective nature. Between February 2013 and December 2017, ninety-six consecutive patients with ischemic stroke underwent intra-arterial mechanical thrombectomy, followed by immediate (<24 hours) postinterventional nonenhanced brain CT (CT_{imme}). The Solitaire (Covidien, Irvine, California) was used as a stent-retriever system for all the patients. Among them, patients who satisfied the following criteria were included in this study: 1) patients who showed newly developed hyperdensity in the affected areas on CT_{imme} ; 2) patients who underwent DWI including B_0 and GRE sequences within 24 hours after intra-arterial mechanical thrombectomy; and 3) patients who underwent follow-up nonenhanced brain CT (CT_{FU}) between 24 and 72 hours after thrombectomy. Based on previous studies,^{5,10} hemorrhagic transformation was defined as a parenchymal hyperdensity in the infarcted area on CT_{imme} that persisted on CT_{FU} . On the other hand, contrast staining was defined as a parenchymal hyperdensity on CT_{imme} that had disappeared on CT_{FU} . The patients were divided into 2 groups based on the findings on CT_{imme} and CT_{FU} (Fig 1). Among them, 14 patients

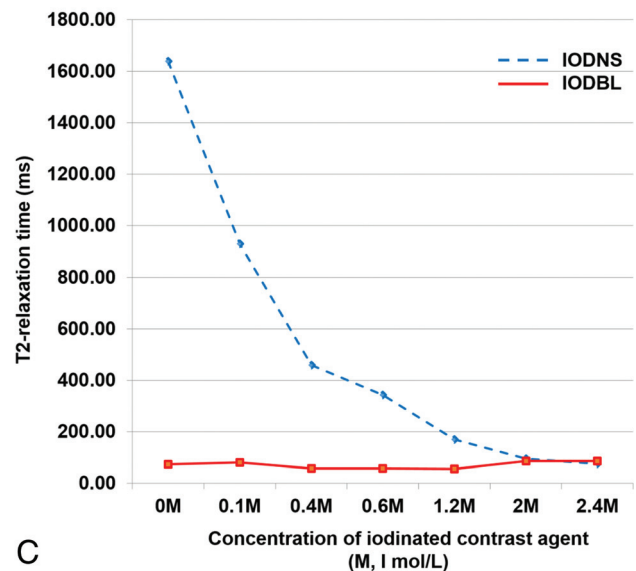
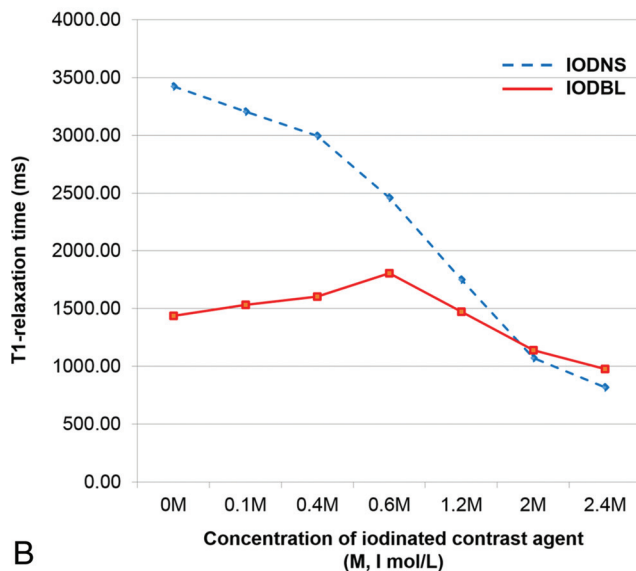
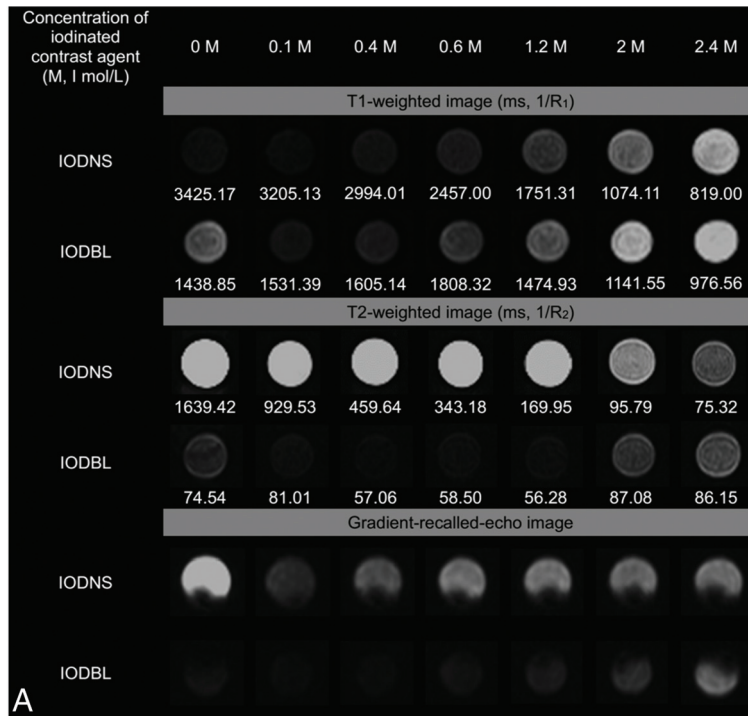


FIG 2. MR signal intensity of IODNS and IODBL on T1-weighted, T2-weighted, and gradient recalled-echo images. **A**, Images from the phantom. **B**, T1-relaxation times of IODNS and IODBL at different concentrations. **C**, T2-relaxation times of IODNS and IODBL according to the concentration of iodinated contrast agents. Visipaque (iodixanol, 320 I mg/mL, 2.5 I mol/L, iso-osmolar) was used as the iodinated contrast agent in this phantom.

(14/17 [82.35%]) also underwent conventional MR imaging, including T1WI and T2WI within 24 hours after intra-arterial mechanical thrombectomy. The type of the hemorrhagic transformation was evaluated on the basis of the European-Australasian Acute Stroke Study (ECASS) criteria.¹¹ Symptomatic intracerebral hemorrhage was defined according to ECASS II.¹² The fate of contrast staining was analyzed using the last imaging study before the discharge.

MR Imaging Acquisition and Analysis of Patients

MR images were acquired using four 3T MR imaging scanners (Prisma, Skyra, and Trio Tim, Siemens; and Achieva, Philips Healthcare, Best, the Netherlands) with a 32- or 64-channel head

coil. Imaging sequences included DWI (B_0 , $b=1000$), GRE imaging, T2WI, and T1WI. The MR imaging parameters were as follows: single-shot echo-planar imaging sequence; TR/TE/matrix = 3590–5970 ms/57–91 ms/128 × 120–192 × 192, $b=0$ and 1000 s/mm², bandwidth = 920–2374 Hz per voxel, 3 signals acquired for DWI; TR/TE/flip angle/matrix = 543–819 ms/12–15 ms/18°–20°/244 × 244–320 × 240 for GRE imaging; TR/TE/flip angle/matrix = 3000–6450 ms/80–118 ms/90°–150°/368 × 353–512 × 358 for spin-echo T2WI; TR/TE/flip angle/matrix = 578–1850 ms/10–12 ms/90°–120°/224 × 224–384 × 269 for fast spin-echo T1WI; section thickness, 4–5 mm (with a gap of 0.5–0.8 mm); and FOV = 179 × 220 or 220 × 220 mm.

Table 1: MR signal intensities of hemorrhagic transformation and contrast staining in B₀ and GRE image^a

	Hemorrhagic Transformation (n = 8)	Contrast Staining (n = 9)	Total (n = 17)	P
B ₀				<.001
Score 1	8 (100.00%)	0 (0.00%)	8 (47.06%)	
Score 2	0 (0.00%)	0 (0.00%)	0 (0.00%)	
Score 3	0 (0.00%)	3 (33.33%)	3 (17.65%)	
Score 4	0 (0.00%)	6 (66.67%)	6 (35.29%)	
GRE				<.001
Score 1	8 (100.00%)	0 (0.00%)	8 (47.06%)	
Score 2	0 (0.00%)	0 (0.00%)	0 (0.00%)	
Score 3	0 (0.00%)	6 (66.67%)	6 (35.29%)	
Score 4	0 (0.00%)	3 (33.33%)	3 (17.65%)	

^a Values are numbers of patients with percentages in parentheses. Score 1, signal intensity was similar to that of the vessel; score 2, signal intensity was lower than that of the gray matter; score 3, signal intensity was similar to that of the gray matter; score 4, signal intensity was higher than that of the gray matter.

Table 2: MR signal intensities of hemorrhagic transformation and contrast staining in T1WI and T2WI^a

	Hemorrhagic Transformation (n = 6)	Contrast Staining (n = 8)	Total (n = 14)	P
T1WI				.042
Score 1	1 (16.67%)	0 (0.00%)	1 (7.14%)	
Score 2	5 (83.33%)	3 (37.50%)	8 (57.14%)	
Score 3	0 (0.00%)	5 (62.50%)	5 (35.71%)	
Score 4	0 (0.00%)	0 (0.00%)	0 (0.00%)	
T2WI				.001
Score 1	6 (100.00%)	0 (0.00%)	6 (42.86%)	
Score 2	0 (0.00%)	0 (0.00%)	0 (0.00%)	
Score 3	0 (0.00%)	3 (37.50%)	3 (21.43%)	
Score 4	0 (0.00%)	5 (62.50%)	5 (35.71%)	

^a Values are numbers of patients with percentages in parentheses. Score 1, signal intensity was similar to that of the vessel; score 2, signal intensity was lower than that of the gray matter; score 3, signal intensity was similar to that of the gray matter; score 4, signal intensity was higher than that of the gray matter.

The imaging analyses for dividing the groups were performed by 1 neuroradiologist (S.-H.Y. with 7 years of clinical experience) using the CT_{imme} and CT_{FU} images. Analyses of the immediate postinterventional MR images were performed by 2 neuroradiologists (B.K.K. and B.K. with 8 and 13 years of clinical experience, respectively) who were blinded to the CT_{FU} data. B₀, DWI, and GRE images of all patients were analyzed and T1WI/T2WI of those who underwent conventional MR imaging were reviewed. MR images, CT_{imme} images, and information concerning the target location were provided to the 2 reviewers. Two reviewers performed visual analysis based on the following criteria that we devised for the study: score 1, signal intensity similar to that of the vessel; score 2, signal intensity lower than that of the gray matter; score 3, signal intensity similar to that of the gray matter; and score 4, signal intensity higher than that of the gray matter.

Statistical Analysis

The Mann-Whitney *U* test was used to compare the medians of continuous variables that were nonparametrically distributed (NIHSS and mRS scores) and ordinal variables (TICI scores, hemorrhagic transformation, and MR signal intensity score), while the unpaired *t* test was used to compare the means of continuous variables (age) between the 2 groups. The Fisher exact test was used to compare categorical variables between the groups. All statistical analyses were performed using SPSS Statistics for Windows, Version 20.0 (IBM, Armonk, New York). A *P* value < .05 was considered statistically significant.

RESULTS

MR Signal Intensities of Various Iodinated Contrast Agents

The MR signal intensities and relaxation times of the 5 different IODNSs in the T1-weighted, T2-weighted, and GRE images are shown in On-line Figs 1–3. All 5 iodinated contrast agents showed a similar tendency of signal intensity change at each concentration. T1- and T2-shortening effects were commonly observed, which became more prominent at high iodine concentrations. At the lowest concentration (0.1 I mg/mL), the T1 values of the 5 different IODNSs ranged from 3205 to 3704 ms. As the concentration increased, the T1-relaxation times progressively decreased to a range of 819–1144 ms at the highest concentration (2.4 I mg/mL). The T2 values of the 5 different IODNSs ranged from 1030–1913 ms at the lowest concentration (0.1 I mg/mL). As the concentration increased, the T2-relaxation times were progressively reduced in all the iodinated contrast agents and ranged from 52–78 ms at the highest concentration (2.4 I mg/mL). In the GRE images, the signal intensity did not show a specific trend according to concentration of the contrast agents.

Comparison of MR Signal Intensities between IODNS and IODBL

MR signal intensities and relaxation times of IODNS and IODBL in the T1-weighted, T2-weighted, and GRE images are shown in Fig 2. At most iodine concentration ranges (0.1–1.2 I mol/L), IODNS could be differentiated from IODBL visually in the T2-weighted and GRE images. On T2WI, the T2 signal intensities of IODBL were darker than those of IODNS in visual assessment. The T2-relaxation times of IODBL (56–87 ms) were lower than those of IODNS (96–1639 ms) at most iodine concentrations (range, 0.1–2.0 I mg/mL) (Fig 2A, -B). On GRE images, IODBL showed dark signal intensity and IODNS showed intermediate signal intensity. There was no specific trend of signal change according to the concentration of the contrast agent (Fig 2A). On T1WI, it was impossible to differentiate IODNS and IODBL (Fig 2C).

Baseline Characteristics of Patients

The clinical characteristics of patients are summarized in On-line Table 1. Among the 17 patients, 8 were classified as having hemorrhagic transformation, and 9, as having contrast staining. No significant difference was observed between the 2 groups. One of 8 patients (12.50%) in the hemorrhagic transformation group showed symptomatic intracerebral hemorrhage. The final outcomes of areas of contrast staining were infarction in 7 patients (7/9 [77.78%]) (On-line Table 2).

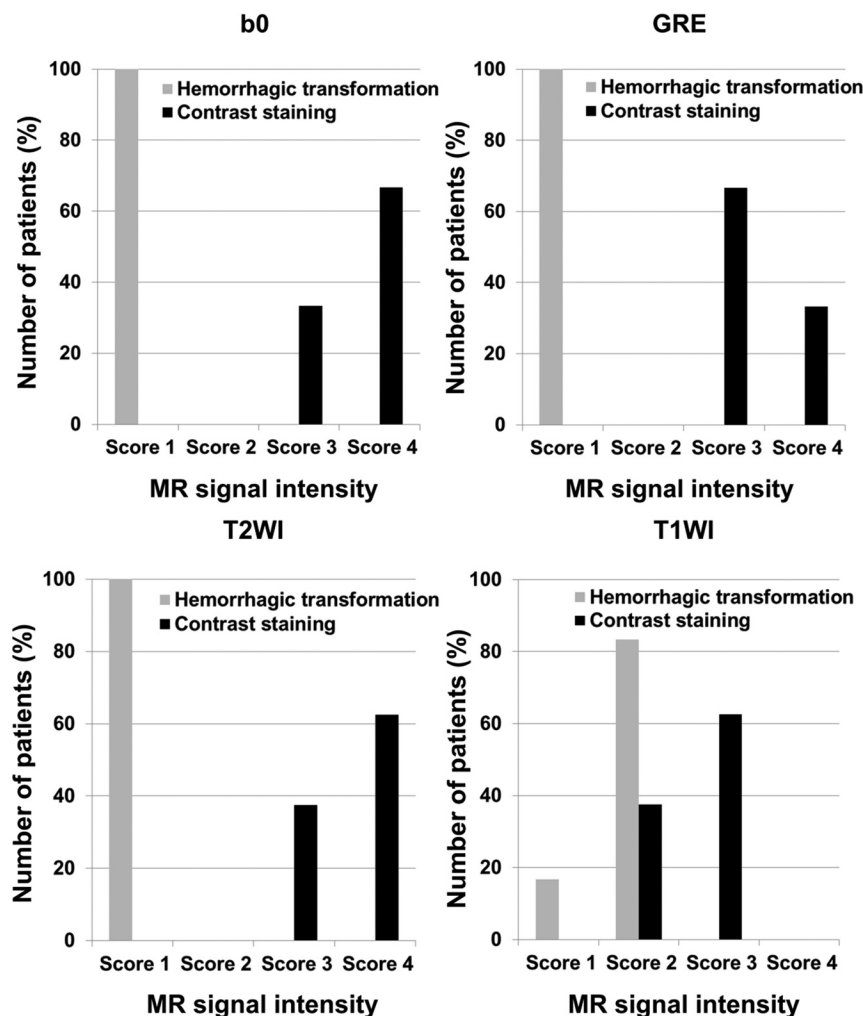


FIG 3. Magnetic signal intensity score of hemorrhagic transformation and contrast staining on B₀, gradient recalled-echo, T2-weighted, and T1-weighted imaging. Score 1, signal intensity was similar to that of the vessel; score 2, signal intensity was lower than that of the gray matter; score 3, signal intensity was similar to that of the gray matter; and score 4, signal intensity was higher than that of the gray matter.

MR Signal Intensities of Hemorrhagic Transformation and Contrast Staining

The MR signal intensity scores of hemorrhagic transformation and contrast staining are summarized in Tables 1 and 2 and Fig 3. Hemorrhagic transformation showed significantly lower visual scores than contrast staining in all MR imaging sequences (B₀, GRE, T1WI, and T2WI) ($P < .05$). All hemorrhagic transformations had a score of 1 (signal intensity was similar to that of the vessel) on B₀, GRE, and T2WI. However, all contrast staining had scores of 3 or 4 (signal intensity was similar to or higher than that of the gray matter). Representative MR images, including B₀, GRE, T2WI, and T1WI, are shown in Fig 4. Hemorrhagic transformation showed a dark signal intensity similar to that of the vessel, and contrast staining demonstrated an iso- or hyper-signal intensity compared with that of the normal gray matter on B₀, GRE, and T2WI.

DISCUSSION

In the present phantom study, the T2WI and GRE sequences could differentiate IODBL from IODNS at most of the iodine

concentrations (0.1–1.2 mol/L). In the exploratory patient study, immediate postinterventional B₀ and GRE images enabled differentiation of contrast staining from hemorrhagic transformation in patients with acute ischemic stroke who underwent endovascular thrombectomy.

The use of DWI for differentiating contrast staining from hemorrhagic transformation has 3 clinical advantages: First, MR imaging is available in almost all hospitals that treat acute ischemic stroke, and DWI and GRE are widely used sequences. Although the usefulness of dual-energy CT for differentiating these entities has been revealed in several previous studies, it cannot be applied in some types of CT scanners.^{6,7,13} Second, B₀-DWI may be used as an alternative to T2WI with a shorter scan time and at a lower cost. Our results demonstrated that B₀ imaging was not inferior to T2WI in differentiating hemorrhagic transformation and contrast staining. Third, $b = 1000$ -DWI could offer information about final infarction size, which influences treatment outcomes of endovascular thrombectomy.

In T2WI and B₀-DWI, contrast staining could be differentiated from hemorrhagic transformation. IODNS demonstrated a T2-shortening effect, but IODBL showed a much stronger T2-shortening effect. These results correspond well with those of earlier studies.^{9,14,15} The mechanism of the T2-shortening effect of the iodinated

contrast agent is not well-known, but the bound water effect and dipole-dipole interaction theories have been suggested as the most important mechanisms.^{16,17} In general, the T2-shortening effect is explained by 3 major mechanisms: paramagnetism, bound water effect, and dipole-dipole interaction.¹⁸ The paramagnetic effect could be excluded because iodinated contrast agents are classified as diamagnetic materials that do not have unpaired electrons.¹⁹ The bound water effect could be the cause of the T1- and T2-shortening effects. This is because neither the iodine nor the benzene ring could influence the relaxation process of water molecules; however, the hydrophilic hydroxyl-containing portion of the iodinated contrast agent can form a hydrogen bond with water.¹⁹ Bound water shows more rapid relaxation than free water; therefore, the bound water effect of the contrast agent may lead to T2-shortening.¹⁸ A dipole-dipole interaction that occurs between 2 adjacent molecules that have different degrees of electronegativity could influence T2-shortening because iodinated contrast agents and water have different degrees of electronegativity. In the phantom study, IODBL showed a much

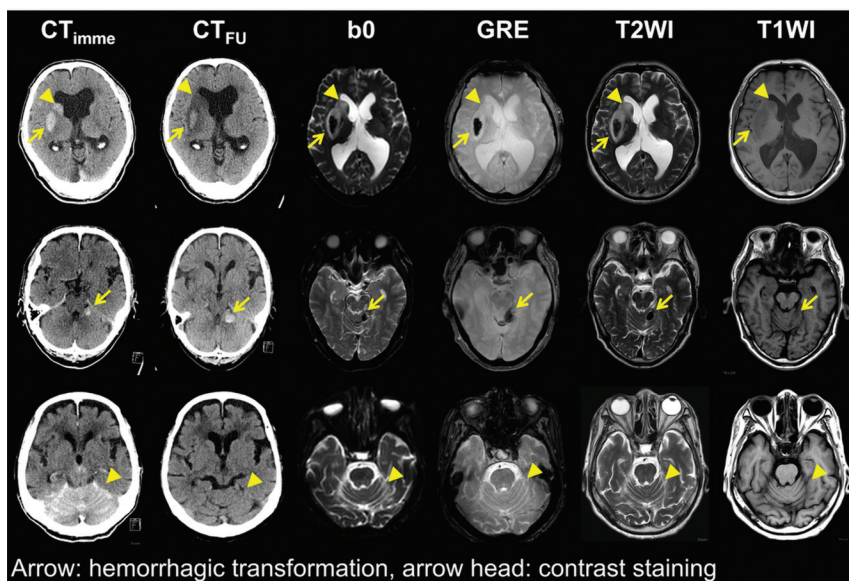


FIG 4. Representative images of hemorrhagic transformation and contrast staining in 3 patients with acute ischemic stroke. *First row:* images of a 66-year-old man with infarction in the territory of the right middle cerebral artery. A persistent hyperdense lesion in the right lentiform nucleus, presumed to be a hemorrhagic transformation (arrow), shows dark signal intensity in the B_0 , gradient recalled-echo, and T2-weighted images. In contrast, a hyperdense lesion in the right caudate nucleus, which is washed out on the follow-up nonenhanced brain CT and presumed to be contrast staining (arrowhead), demonstrates a high signal intensity in the B_0 , GRE, and T2-weighted images. This patient was grouped into the hemorrhagic transformation group, and the lesion in the lentiform nucleus was analyzed. *Middle row:* images of a 68-year-old man with infarction in the region of the right superior cerebellar artery. A persistent hyperdense lesion in the left cerebellum, presumed to be hemorrhagic transformation (arrow), shows dark signal intensity in the B_0 , GRE, and T2-weighted images. *Lower row:* images of an 88-year-old woman with bilateral cerebellar infarction. A hyperdense lesion in the bilateral upper cerebellum, which disappeared on CT_{FU} and was presumed to be contrast staining (arrowhead), demonstrates iso-signal intensity in the B_0 , GRE, and T2-weighted images.

stronger T2-shortening effect than IODNS. These results could be explained by 2 hypotheses^{9,14,15}: First, the T2-shortening effect of blood caused by the paramagnetic mechanism was much stronger than that of the bound water and dipole-dipole interaction effects of the iodinated contrast agent. Second, the bound water and dipole-dipole interaction effects of the iodinated contrast agent were weaker in the blood-mixed environment than in the water-mixed environment. Under these mechanisms, the more powerful T2-shortening effect of IODBL made it possible to distinguish IODNS from IODBL. In patient data, this effect also applied not only to T2WI but also to B_0 -DWI; thus, hemorrhagic transformation and contrast staining could be differentiated using immediate postinterventional DWI.

In the GRE images, hemorrhagic transformation could be differentiated from contrast staining by its strong positive susceptibility. IODNS showed a more minimal signal drop than pure water in the phantom study. This effect did not show a specific trend according to the concentration or kind of contrast agent. This phenomenon is difficult to explain because iodinated contrast agents are classified as diamagnetic materials that do not have unpaired electrons. One hypothesis is that diamagnetic materials are repelled by magnetic fields. Therefore, these materials possibly reduce the intensity of the magnetic fields only minimally and cause a minimal signal drop. However, this minimal signal drop could not be visualized on patients' imaging data. This result agrees with that of a previous animal study.⁹

Because blood has strong positive susceptibility, hemorrhagic transformation was well-distinguished from contrast staining in the GRE images.

Five kinds of commonly used non-ionic iodinated contrast agents were evaluated to reveal the effect of the side chains that are different in each contrast agent. Our study showed no significant difference in the T1 and T2 values among the different contrast agents at the same concentration. This is in concordance with the results of previous studies.^{9,16} The absence of a definite difference in the T1 and T2 values is probably because all kinds of iodinated contrast agents used in our study were nonionic. A minor difference in signal intensity among the contrast agents may be caused by their different side chains.

Several studies have reported the clinical relevance of newly developed parenchymal hyperdensity after mechanical thrombectomy, which is not associated with poor prognosis or symptomatic hemorrhage.^{3,10} In our study, the median mRS score at 90 days in the overall population that underwent mechanical thrombectomy ($n = 86/96$; 10 patients lost to follow-up) was 3.0 (interquartile range, 2.0–5.0). It is similar

to that in our final study population, which demonstrated newly developed parenchymal hyperdensity (3.0 [interquartile range 2.0–3.0]). In addition, only 1 of 17 cases showed symptomatic intracerebral hemorrhage in the present study. Regarding the longitudinal outcomes of areas of contrast staining, approximately 80% finally progressed to infarction in this study. This result is in close agreement with those of the other studies.^{10,20}

Our study has several limitations. First, the number of patients included in our retrospective study was small. Large-scale prospective studies are needed to validate the findings of this study. Second, oxygen saturation was not measured in our study; hence, the exact chemical status of blood could not be presented. Third, we cannot predict the effect of anticoagulating agents, such as heparin, present in the tubes containing the blood samples on MR imaging.

CONCLUSIONS

According to our preliminary results, contrast staining might be differentiated from hemorrhagic transformation using an immediate postinterventional DWI protocol including GRE imaging.

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