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Bone Subtraction Iodine Imaging Using Area Detector CT for Evaluation of Skull Base Invasion by Nasopharyngeal Carcinoma

 T. Hiyama,  H. Kuno,  K. Sekiya,  S. Tsushima,  O. Sakai,  M. Kusumoto, and  T. Kobayashi



ABSTRACT

BACKGROUND AND PURPOSE: Conventional CT has generally lower detectability of bone marrow invasion than MR imaging due to lower tissue contrast. The purpose of this study was to compare the diagnostic performance of conventional CT alone or in combination with bone subtraction iodine imaging using area detector CT for the evaluation of skull base invasion in patients with nasopharyngeal carcinoma.

MATERIALS AND METHODS: Forty-four consecutive patients who underwent contrast-enhanced CT using 320-row area detector CT and contrast-enhanced MR imaging for nasopharyngeal carcinoma staging between April 2012 and November 2017 were enrolled in this retrospective study. Bone subtraction iodine images were generated by subtracting pre- and postcontrast volume scans using a high-resolution deformable registration algorithm. Two blinded observers evaluated skull base invasion at multiple sites (sphenoid body, clivus, bilateral base of the pterygoid process, and petrous bone) using conventional CT images alone or in combination with bone subtraction iodine images. Examination of MR and CT images by an experienced neuroradiologist was the reference standard for evaluating sensitivity, specificity, and area under the receiver operating characteristic curve.

RESULTS: Twenty-six patients (59%) showed skull base invasion at 84 sites on the reference standard. Conventional CT plus bone subtraction iodine images showed higher sensitivity (92.9% versus 78.6%, $P = .02$) and specificity (95.6% versus 86.1%, $P = .01$) than conventional CT images alone for evaluating skull base invasion. The area under the receiver operating characteristic curve for conventional CT plus bone subtraction iodine (0.98) was significantly larger ($P < .001$) than the area under the receiver operating characteristic curve for conventional CT alone (0.90).

CONCLUSIONS: Conventional CT plus bone subtraction iodine performs more closely to the accuracy of combining CT and MR imaging compared with conventional CT alone.

ABBREVIATIONS: AUC = area under the receiver operating characteristic curve; BSI = bone subtraction iodine; CCT = conventional CT; NPC = nasopharyngeal carcinoma

Nasopharyngeal carcinoma (NPC), arising from the epithelial lining of the nasopharynx, has a propensity to invade the skull base just above the nasopharynx. Skull base invasion indicates a tumor stage of at least T3 according to the eighth edition of

the American Joint Committee on Cancer staging system.¹ NPC is treated mainly by radiation therapy, with or without chemotherapy. Intensity-modulated radiation therapy has gradually become the standard treatment for NPC because of its superior tumor target conformity and significantly improved localization.^{2,3} As the spatial accuracy of dose distribution improves, a more precise evaluation of the spatial extent of NPC is required.

MR imaging offers excellent soft-tissue contrast and is useful for the diagnosis, staging, and evaluation of tumor extent.⁴⁻⁷ It is

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well-established that MR imaging is better than CT at identifying invasion of the skull base.⁸⁻¹¹ CT can detect skull base involvement manifesting as lytic or sclerotic lesions but has lower sensitivity than MR imaging due to lower tissue contrast and lower detectability of bone marrow invasion. However, CT is often the primary imaging technique for radiation therapy planning and dose computation and may be the only option for patients with contraindications to MR imaging such as intracranial or orbital metallic foreign bodies and MR imaging–unsafe pacemaker devices, or for patients who cannot tolerate MR imaging because of claustrophobia.

Currently, digital subtraction angiography-like bone subtraction iodine (BSI) imaging with 160-mm-wide area detector CT is used in some musculoskeletal and neurologic applications.¹²⁻¹⁴ According to Gondim Teixeira et al,¹² BSI imaging with area detector CT showed high performance for the visual identification of bone marrow enhancement adjacent to lytic bone lesions. This technique reduces spatial mismatch by using volume scanning with wide area detector CT and a high-resolution deformable registration algorithm, enabling identification of contrast enhancement in the bone marrow. We hypothesized that BSI imaging might be useful for detecting skull base invasion and accurately assessing the extent of bone invasion by the NPC.

Hence, the purpose of this retrospective study was to compare the diagnostic performance of conventional CT (CCT) alone and in combination with BSI imaging using area detector CT for the evaluation of skull base invasion in patients with NPC.

MATERIALS AND METHODS

Study Population

Our institutional review board at National Cancer Center Hospital East approved this retrospective study. The requirement to obtain written informed consent was waived. Between April 2012 and November 2017, forty-seven consecutive newly diagnosed patients with histologically proved NPC underwent contrast-enhanced CT for cancer staging before treatment. Among them, 46 patients also underwent contrast-enhanced 3T MR imaging before treatment. Two of the 46 patients were excluded because of unavailable volume data needed for subtraction reconstruction. The remaining 44 patients (28 men, 16 women; age range, 18–79 years; mean age, 60 years) were enrolled in this study. Of the 44 patients, 29 (65.9%) had nonkeratinizing squamous cell carcinoma and 8 (18.2%) had keratinizing squamous cell carcinoma. The detailed clinical profiles are summarized in Table 1. Tumor stage was determined according to the seventh edition of the American Joint Committee on Cancer staging system.¹⁵

Digital Subtraction Angiography-Like BSI Imaging Techniques

All CT studies were performed using a 320–detector row CT system with a detector width of 160 mm (Aquilion ONE Vision; Canon Medical Systems, Otawara, Japan), with the following parameters: 120 kV, 120 effective mAs (milliampere-second), 0.5-second rotation time, 160-mm collimation. The average CT dose index was 25.2 mGy. Patients received a 100-mL injection of 300 mg I/mL of iodinated contrast medium (iopamidol; Teva Takeda Yakuhin, Koka, Japan) at a rate of 2.5 mL/s into an antecubital

Table 1: Summary of patient characteristics

Characteristics	No.	%
Age (yr)		
Mean	60	
Range	18–79	
Sex		
Female	16	36.0%
Male	28	64.0%
Histopathology		
Nonkeratinizing carcinoma	29	65.9%
Differentiated	8	
Undifferentiated	19	
Unknown	2	
Keratinizing carcinoma	8	18.2%
Unknown	7	15.9%
TNM (7th AJCC)		
T1	8	18.2%
T2	10	22.7%
T3	4	9.1%
T4	22	50.0%
N0	3	6.8%
N1	16	36.4%
N2	13	29.5%
N3a	1	2.3%
N3b	11	25.0%
M0	41	93.2%
M1	3	6.8%
Subsite		
Posterior superior	12	27.3%
Lateral wall	32	72.7%

Note:—TNM indicates tumor, node, metastasis tumor stage; AJCC, American Joint Committee on Cancer.

vein through a 22-ga cannula. Scans were started 7 (mask volume) and 70 seconds (postcontrast volume) after the start of the injection in an intermittent acquisition mode with no table feed. During volume scanning, the patient's head was fixed to the bed of the CT with a headband and neck collar (Stifneck Select; Laerdal, Stavanger, Norway) (On-line Fig 1).

Two volume datasets (7- and 70-second CT) were reconstructed using a high-resolution deformable registration algorithm. The mask volume was subtracted from the postcontrast volume using the ^{SURE}Subtraction application (Canon Medical Systems). The high-resolution deformable registration algorithm is described in detail in the On-line Appendix and On-line Fig 2.¹⁶ Axial and coronal CCT images with soft-tissue (window level 65, window width 330) and bone (window level 650, window width 3000) windows, and axial and coronal BSI images (window level 40, window width 180) were reconstructed with a 2-mm slice thickness, 512 × 512 matrix, and 16-cm FOV. The CCT and BSI images were reconstructed to yield precisely matching slices.

Image Interpretation

Two independent radiologists (with 12 years [H.K.] and 24 years [T.K.] of experience in oncologic diagnostic radiology), blinded to the patients' clinical histories and to the images from the other technique, independently analyzed the images. The CCT images and combined CCT-plus-BSI images were evaluated using a 5-point scale for calculating the area under the receiver operating characteristic curve (AUC) and weighted κ statistics. For CCT images, findings for skull base invasion were considered negative when the tumor was separated from the skull base (score 1, defi-

nately negative) or was only in contact with the skull base (score 2, probably negative). Findings of skull base invasion were considered present when erosion or sclerosis (score 3, possibly positive), erosion and sclerosis (score 4, probably positive), or invasion into the bone marrow (score 5, definitely positive) was present. For combined analysis of CCT and BSI images, we scored skull base invasion using the BSI image in addition to the CCT image. If the BSI image showed definitive bone enhancement continuous with the tumor, we scored it as grade 5 (definitely positive); the absence of enhancement was scored as grade 2 (probably negative). If the bone marrow enhancement was equivocal or impossible to estimate, we gave scores of 2, three (possibly positive), or 4 (probably positive) based on the confidence level of enhancement on BSI images and findings on CCT. By means of a workstation (Shade Quest View R; Yokogawa Electric, Tokyo, Japan), the images were presented in random order in 2 sessions, initially with CCT alone (soft-tissue and bone window), followed 4 weeks later by a combination of CCT and BSI images. The readers were able to generate fusion images of the bone window and BSI images. Skull base invasion was evaluated at 6 sites on the skull base (sphenoid body, clivus, bilateral pterygoid process, and bilateral petrous apex). The final score for the skull base invasion was determined by a consensus between the 2 readers.

Standard of Reference

Owing to the difficulty in obtaining histopathologic confirmation of skull base invasion, a combination of MR imaging and CT features observed by an experienced neuroradiologist (T.H., 12 years of experience in neuro-/head and neck radiology) who was not involved in image interpretation in this study but made reports clinically in some cases was used as the reference standard for evaluating sensitivity, specificity, and the AUC for skull base invasion. The MR imaging protocol is discussed in the On-line Appendix. All patients underwent MR imaging and CT examinations within a median of 5 days (range, 0–23 days).

MR Imaging and CT Diagnostic Criteria for Skull Base Invasion

Findings of skull base invasion were considered positive in cases in which the skull base had signals similar to those of the adjacent tumor on all pre- and postcontrast T1-weighted images in the cortical bone and bone marrow space on the MR image (low signal intensity on a T1-weighted image and contrast enhancement on the postcontrast T1-weighted image with fat suppression).^{8,9,17–21} We performed evaluations mainly on the basis of the precontrast 3D T1-weighted Dixon in-phase image and the postcontrast 3D T1-weighted Dixon water image. Other sequences were also used for identifying tumor location. CCT was used for the evaluation of bone cortex because CT is superior to MR imaging for the detection of bone cortex invasion. When CT and MR image findings were mismatched for bone marrow invasion, the diagnosis obtained on the basis of MR imaging was used.

Statistical Analysis

For estimating the sensitivity and specificity of both modalities for the detection of skull base invasion, we considered diagnostic confidence scores of >3 as positive diagnoses and generated con-

tingency tables separately for each site on the skull base. For comparisons of sensitivity and specificity, the McNemar test and generalized estimating equations were used to take into account correlations between multiple sites in the same patient.²² The overall diagnostic performance was quantified by the area under the receiver operating characteristic curve using a 5-point scale. Interreader agreement between the independent evaluations of the 2 readers for the scores based on the CCT-alone images and the CCT-plus-BSI images was estimated by weighted κ statistics (weight = 2). This was to account for the fact that differences of >1 point between the scores of the 2 readers were more important than smaller differences.²³ Commercial software (STATA, Version 12.1; StataCorp, College Station, Texas) was used. $P < .05$ was considered a significant difference.

RESULTS

Skull Base Invasion According to the Reference Standard Findings

All CCT and BSI images generated from the 2-volume datasets were considered of diagnostic image quality. In total, we examined 264 sites (44 in the sphenoid body, 44 in the clivus, 88 in the pterygoid process, and 88 in the petrous apex) from 44 patients. Of these 264 sites, skull base invasion was present at 84 sites (31.8%) according to the reference standard findings. A total of 26 patients (59.1%) showed skull base invasion. Bone sclerosis was observed in 21 (47.7%) of the 44 patients, and gross skull base invasion into the bone marrow was observed in 18 (40.9%) of 44 patients. Skull base invasion was present at 22/44 sphenoid body sites (50.0%), 20/44 clivus sites (45.5%), 10/44 right base of the pterygoid process sites (22.7%), 8/44 left base of the pterygoid process sites (18.2%), 12/44 right petrous bone sites (27.3%), and 12/44 left petrous bone sites (27.3%).

Differentiation of Imaging Findings between CCT Alone and CCT-Plus-BSI Imaging

The results of the image interpretation and diagnostic performance overall and at each site on the skull base for the CCT-alone and CCT-plus-BSI imaging are summarized in Table 2. Among the 84 skull base invasions, 66 (78.6%) were correctly detected by CCT alone and 18 (21.4%) produced false-negative findings (4 of the sphenoid body, 9 of the clivus, 1 base of the pterygoid process, and 4 of the petrous apex). With use of both CCT and BSI images, however, the number of false-negative findings decreased from 18 to 6 because the BSI images demonstrated iodine enhancement at the skull base without obvious cortical destruction. Figure 1 shows a representative case of a false-negative finding on CCT alone. On CCT images, extensive destruction or sclerosis of the skull base was unclear, but the BSI images clearly demonstrated iodine distribution within soft tissue and bone (both cortex and bone marrow space) continuous with the tumor. Seventy-four true-positive sites on CCT-plus-BSI had an intensity similar to that of the tumor on T2-weighted images. The remaining 4 cases showed hyperintensity on T2-weighted images compared with the primary tumor. Six (7.1%) false-negative diagnoses of 84 sites remained even after examination of BSI images, due to failure to detect visible iodine enhancement in the bone marrow continuous with the tumor. Among these 6 false-negative diagnoses, 4

Table 2: Comparison between CCT images alone and CCT-plus-BSI images of skull base invasion^a

Parameter	TP ^b	TN ^b	FN ^b	FP ^b	Sensitivity (%)	P Value	Specificity (%)	P Value	PPV (%)	NPV (%)
All sites										
CCT alone	66	155	18	25	79 (68–87)	.016 ^c	86 (80–90)	.010 ^c	73	90
CCT-plus-BSI	78	172	6	8	93 (85–97)		96 (91–98)		91	97
Sphenoid body										
CCT alone	18	14	4	8	82 (60–95)	.625	64 (41–83)	.039 ^d	69	78
CCT-plus-BSI	20	21	2	1	91 (71–99)		95 (77–100)		95	91
Clivus										
CCT alone	11	22	9	2	55 (32–77)	.031 ^d	92 (73–99)	1.000	85	71
CCT-plus-BSI	17	22	3	2	85 (62–97)		92 (73–99)		89	88
Base of the pterygoid process										
CCT alone	17	60	1	10	94 (73–100)	.157	86 (75–93)	.012 ^c	63	98
CCT-plus-BSI	18	68	0	2	100 (81–100)		97 (90–100)		90	100
Petrous apex										
CCT alone	20	59	4	5	83 (63–95)	.221	92 (83–97)	.306	80	94
CCT-plus-BSI	23	61	1	3	96 (79–100)		95 (87–99)		88	98

Note:—FN indicates false-negative findings; FP, false-positive findings; NPV, negative predictive value; PPV, positive predictive value; TN, true-negative findings; TP, true-positive findings.

^a Numbers in parentheses are 95% confidence intervals.

^b Data are numbers of findings.

^c $P < .05$, according to the generalized estimating equations that accounted for the multiple observations within patients.

^d $P < .05$, as determined with the McNemar test.

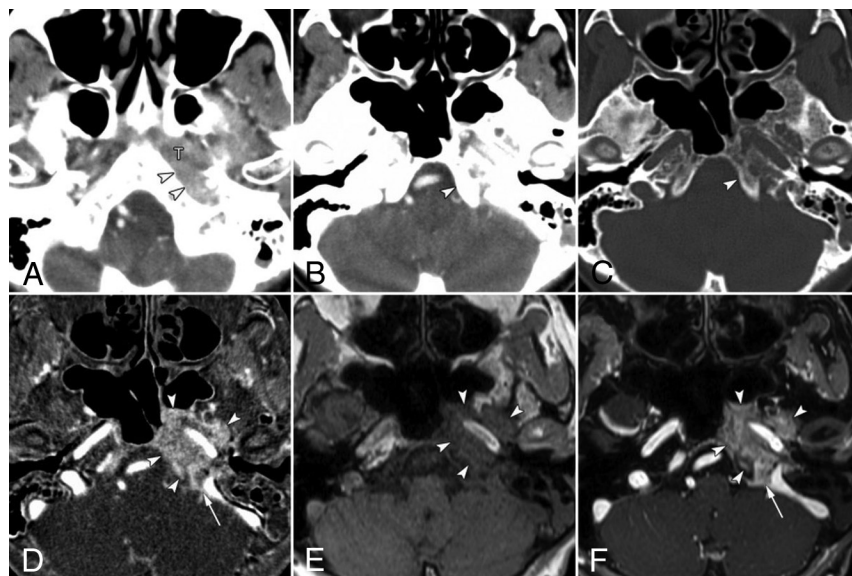


FIG 1. False-negative findings for skull base invasion by conventional CT images alone in a 74-year-old woman with nasopharyngeal carcinoma. A, Axial contrast-enhanced CCT image (soft-tissue window) shows nasopharyngeal tumor (T) spread into the lateral soft tissue around the foramen lacerum (arrowheads). CCT images at the skull base level (B, soft-tissue window; C, bone window) show no destruction of the skull base at the clivus (arrowhead). D, Bone subtraction iodine image shows remarkable skull base invasion into the bone marrow space such as the clivus, petrous apex, and sphenoid bone (arrowheads) with intracranial extension at the jugular foramen (arrow). A corresponding slice on a T1-weighted image (E) and fat-suppressed T1-weighted image after gadolinium administration (F) show tumor invading the clivus (arrowheads) and spread into the jugular foramen (arrow).

sites in 1 patient were not detected because the tumor showed a weak enhancement with density similar to that of normal bone marrow.

A total of 25 (13.9%) false-positive findings (8 of the sphenoid body, 2 of the clivus, 10 of the pterygoid process, and 5 of the petrous apex) of 180 sites without skull base invasion were observed on CCT-alone images, whereas 8 (4.4%) false-positive findings (1 sphenoid body, 2 of the clivus, 2 of the pterygoid process, and 3 of the petrous apex) were observed on CCT-plus-

BSI images. The number of sites with false-positive findings decreased from 25 to 8 on CCT-plus-BSI imaging because the BSI images could detect an absence of corresponding enhancement in the sclerotic regions indicated on the CCT images. Figure 2 shows a case with a false-positive finding on CCT alone with sclerotic change. Two of 8 false-positive sites (1 of the clivus and 1 of the petrous apex) seen on CCT-plus-BSI were probably observed due to enhancement of normal red bone marrow in a young patient in her 30s, and 1 site (sphenoid body) was observed due to misidentifying noise as contrast enhancement. The other 5 false-positive findings seen on CCT-plus-BSI were caused by equivocal enhancement in the BSI images and were scored mainly on the basis of erosion or sclerosis observed on the CCT images.

Diagnostic Performance of CCT Alone and CCT-Plus-BSI Imaging

In an analysis of all sites taken together, the sensitivity of CCT-plus-BSI (93%; 95% CI, 85%–97%) for the detection of

skull base invasion was significantly higher ($P = .02$) than that of CCT alone (79%; 95% CI, 68%–87%). If we split the analysis by site, for the clivus the sensitivity of CCT-plus-BSI was significantly higher ($P = .03$) (85%; 95% CI, 62%–97%) than that of CCT alone (55%; 95% CI, 32%–77%). For the other sites, the sensitivity for CCT-plus-BSI was higher than that for CCT alone, but none of the differences were significant: sphenoid body ($P = .63$; 91% for CCT-plus-BSI versus 82% for CCT-alone), pterygoid process ($P = .16$; 100% versus 94%), and petrous apex ($P = .22$; 96% versus 83%).

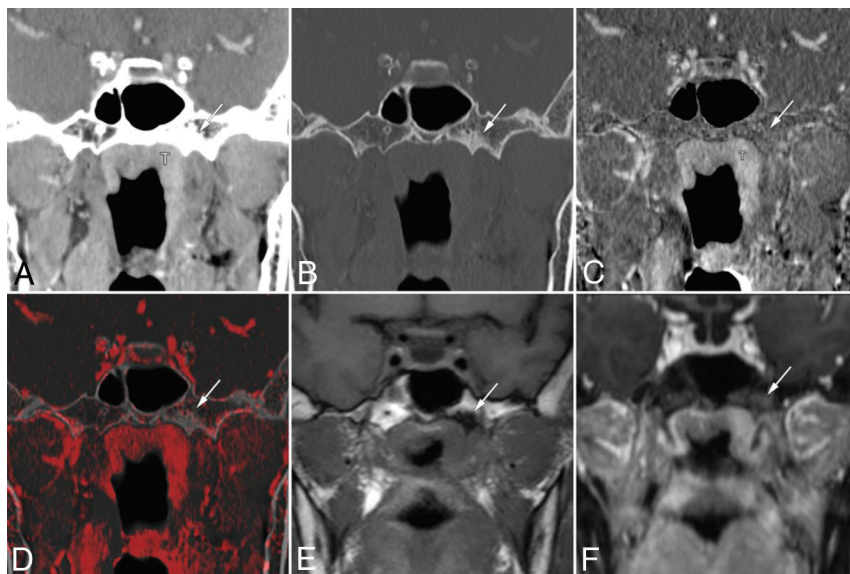


FIG 2. False-positive findings at the base of the left pterygoid process on conventional CT images alone in a 63-year-old woman with nasopharyngeal carcinoma. Coronal contrast-enhanced CCT images (A, soft-tissue window; B, bone window) show nasopharyngeal tumor (T) and bone sclerosis at the left base of the pterygoid process (arrow). The case was given a score of 3 based on CCT images alone. Bone subtraction iodine image (C) and color fusion image (D) clearly show no enhancement in the sclerotic area (arrow). E, A corresponding slice on the T1-weighted image shows low signal intensity due to sclerosis (arrow). F, Fat-suppressed T1-weighted images after gadolinium administration show contrast enhancement of the tumor mass and poor enhancement of the pterygoid process (arrow). This was considered a case of clinical T2 category disease without skull base invasion and was treated by chemoradiotherapy.

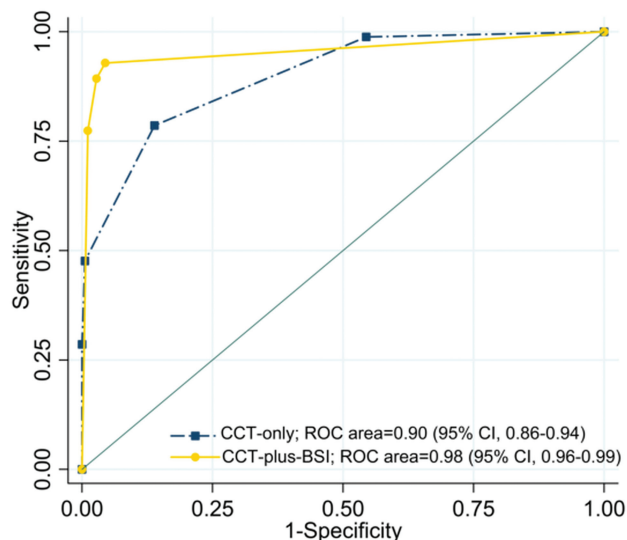


FIG 3. Receiver operating characteristic curves and corresponding areas under the curve for the prediction of skull base invasion. The AUC for CCT-plus-BSI imaging was significantly larger (AUC = 0.98 [$P < .001$]) than that for CCT imaging alone (AUC = 0.90).

The specificity of CCT-plus-BSI (96%; 95% CI, 91%–98%) for the detection of skull base invasion was significantly higher ($P = .01$) than that of CCT alone (86%; 95% CI, 80%–90%) in the analysis of all sites taken together. When we considered each site separately, the specificity of sphenoid body and pterygoid process detection was significantly higher ($P = .04$ and $P = .012$, respectively) in the case of CCT-plus-BSI (sphenoid body: 95%; 95% CI, 77%–100%; pterygoid process: 97%; 95% CI, 90%–100%) than

that of CCT alone (sphenoid body: 64%; 95% CI, 41%–83%; pterygoid process: 86%; 95% CI, 75%–93%). The specificity of CCT-plus-BSI was the same or higher than that of CCT alone at the other sites as well, but none of the differences were significant (clivus: $P = 1.00$, 92% for CCT-plus-BSI versus 92% for CCT-alone; petrous apex: $P = .31$, 95% versus 92%).

The receiver operating characteristic curves for skull base invasion and the corresponding AUCs for diagnosis based on CCT-plus-BSI and CCT-alone are shown in Fig 3. The AUC for CCT-plus-BSI was significantly larger (AUC = 0.98, $P < .001$) than the AUC for CCT alone (AUC = 0.90).

Interobserver Reproducibility

The interreader agreement of the 2 readers for CCT alone and for CCT-plus-BSI was assessed with quadratic weighted statistics, with the following results: agreement of 0.82 (95% CI, 0.53–1.00) and 0.86 (95% CI, 0.56–1.00), respectively, for the sphenoid body; agreement of 0.84 (95% CI, 0.55–1.00) and 0.83

(95% CI, 0.54–1.00), respectively, for the clivus; agreement of 0.85 (95% CI, 0.57–1.00) and 0.86 (95% CI, 0.58–1.00), respectively, for the right base of the pterygoid process; agreement of 0.82 (95% CI, 0.55–1.00) and 0.81 (95% CI, 0.53–1.00), respectively, for the left base of the pterygoid process; agreement of 0.81 (95% CI, 0.52–1.00) and 0.89 (95% CI, 0.59–1.00), respectively, for the right petrous apex; agreement of 0.85 (95% CI, 0.57–1.00) and 0.86 (95% CI, 0.58–1.00), respectively, for the left petrous apex.

DISCUSSION

The results of our study demonstrate that the combined analysis of CCT and BSI images showed a better diagnostic performance than the analysis of CCT images alone in the evaluation of skull base invasion in patients with NPC. These results suggest that CCT-plus-BSI images potentially allow an assessment closely resembling that provided by combining CT and contrast-enhanced MR imaging. High sensitivity could be achieved because CCT-plus-BSI improves the detection of tumor spread within the skull base (cortical bone and bone marrow), especially in the clivus. Another factor contributing to the improved specificity was that CCT-plus-BSI reduced the overestimation caused by sclerotic parts such as the sphenoid body and pterygoid process, which may reflect the bone response to tumor proximity. The differences in the diagnostic performance of each site may be due to the amount of bone marrow, the thickness of the bone affected by pneumatization, and the frequency of sclerosis. These results may be particularly useful for improving the accuracy for radiation therapy treatment planning and primary tumor staging. Further-

more, CCT-plus-BSI imaging offers a benefit for patients with contraindications to MR imaging due to metallic foreign bodies, MR imaging–unsafe pacemaker devices, or claustrophobia.

CT is an excellent technique for the evaluation of bone details, particularly for the evaluation of cortical bone invasion. However, it is still challenging to assess tumor extent in the bone marrow using CCT imaging without contrast-enhanced MR imaging because of low contrast resolution and beam-hardening artifacts produced by the bone cortex. MR imaging is superior to CT in the detection of skull base involvement.^{8–11} Several studies have used MR imaging to examine abnormalities of the skull base in patients with NPC.^{17–21,24} Lu et al²⁰ reported worse prognosis when ≥ 2 sites of skull base invasion were found on MR imaging. Other groups found that the prognosis varied depending on the sites of skull base invasion.^{17,21,24} Therefore, from the perspective of prognosis, comprehensive assessment is needed, including the sites and spatial extent within the skull base. BSI images have the potential to detect enhancement in the bone marrow and may complement CCT in assessing bone invasion.

Shatzkes et al²⁵ reported that sclerotic findings in the pterygoid process are detected on CT in 60% of cases of untreated NPC. These findings may indicate present or imminent skull base invasion and may be used for tumor staging and the formulation of intensity-modulated radiotherapy fields. These sclerotic changes may be a sensitive indicator of skull base invasion, but they are not specific because sclerosis can also be caused by inflammatory or reactive changes.^{26,27} Recently, there have been several reports of the use of dual-energy CT for the diagnosis of bone marrow edema in patients with bone fractures^{28–30} and for the detection of bone marrow involvement in patients with multiple myeloma.³¹ However, with current dual-energy CT systems and material decomposition algorithm, dual-energy CT technology cannot clearly distinguish bone from iodinated contrast.^{32,33} Thus, calcium (bone) remains visible on the iodine map. BSI images generated by area detector CT allow bone removal (both cortical and trabecular) without affecting the visualization of contrast enhancement in a nonlytic bone background.^{12–14} BSI imaging may be helpful for the diagnosis of bone invasion with or without erosive changes in cortical bone.

There are limitations to our study. The first is the absence of histopathologic verification of the findings of skull base invasion because the difficulty in accessing the skull base precludes surgical confirmation and almost all patients were treated with chemoradiotherapy. According to a study of MR imaging findings for laryngeal cartilage invasion, contrast enhancement is also caused by reactive inflammation, edema, and fibrosis in close proximity to the tumor.³⁴ Therefore, there is no clear consensus on whether the contrast enhancement on BSI images was caused by tumor invasion or inflammation. These issues need to be examined at other primary sites such as the mandibular bone or maxillary bone in future studies. The second potential limitation is that skull base invasion was assessed only visually, without quantitative measurement of iodine concentrations. Therefore, potentially confounding effects of interreader error, including display settings, may be present. Moreover, the degree by which tumor and bone marrow enhancement influence the quality and diagnostic per-

formance of BSI images remains unclear and needs to be evaluated in future studies.

CONCLUSIONS

The combined analysis of CCT and BSI images generated from 320–row area detector CT has the potential to improve diagnostic performance in the evaluation of skull base invasion by NPC. BSI images can provide additional contrast resolution for bone assessment. Although there is no direct comparison between the underlying tumor histopathology and the results of BSI imaging, CCT-plus-BSI imaging may be useful for accurate staging of the tumor and may be helpful for patients with contraindications for MR imaging.

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